Preprocessing of fMRI data (basic)

Practical session SPM Course 2016, Zurich

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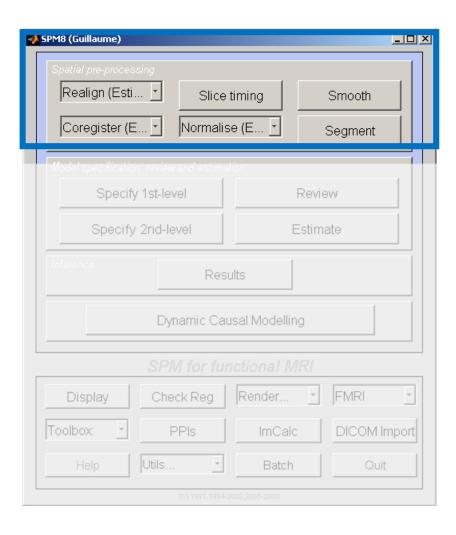


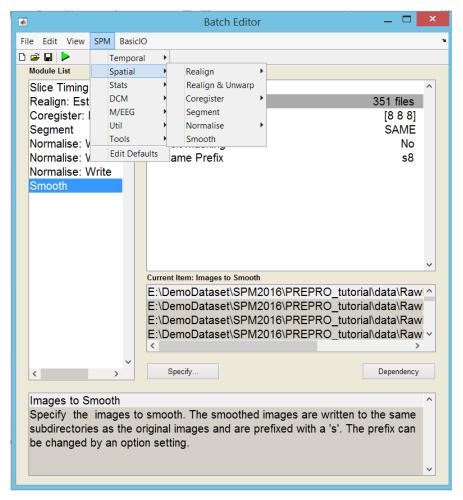
Goals of this session

- Go through a preprocessing pipeline in SPM.
- Learn how to check whether some basic steps worked.
- Some basic file operations in SPM.
- Save, load and modify batches
- How to make your own preprocessing script.
- Answers to "all" your questions.



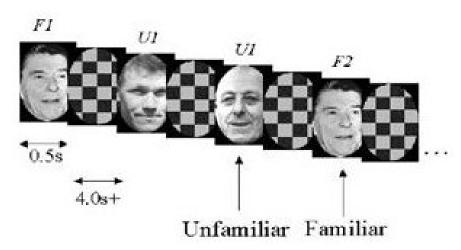
Preprocessing tools on the SPM GUI and Batch Editor

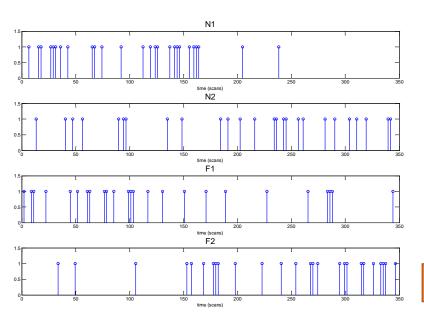






The Dataset: Event-related fMRI





- Goal: Investigate Repetition Suppression
- How: Each face presented twice during the session, 26 famous and 26 nonfamous faces
 - 2x2 factorial design
 - Factor Fam(iliarity): long-term memory,
 - Level: Famous or Unfamous
 - Factor Rep(itition)
 - Level: 1 or 2
 - Task: Button press to decide fame

Stimulus Onsets

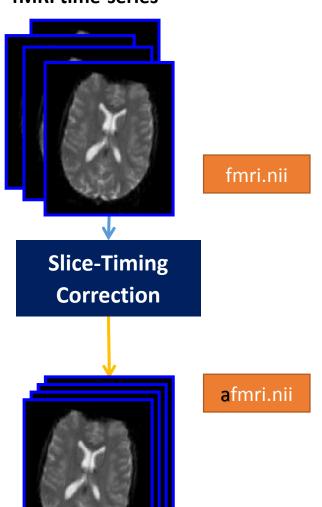
all_conditions.mat

R. Henson et al., Cereb Cortex 2002

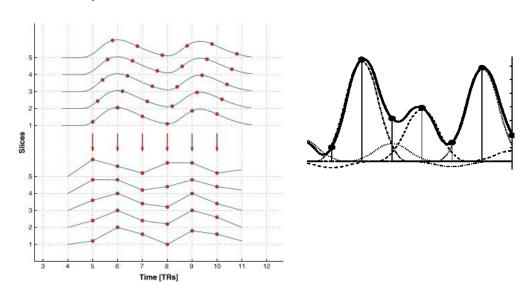


Slice-Timing Correction (Temporal Preproc)

fMRI time-series

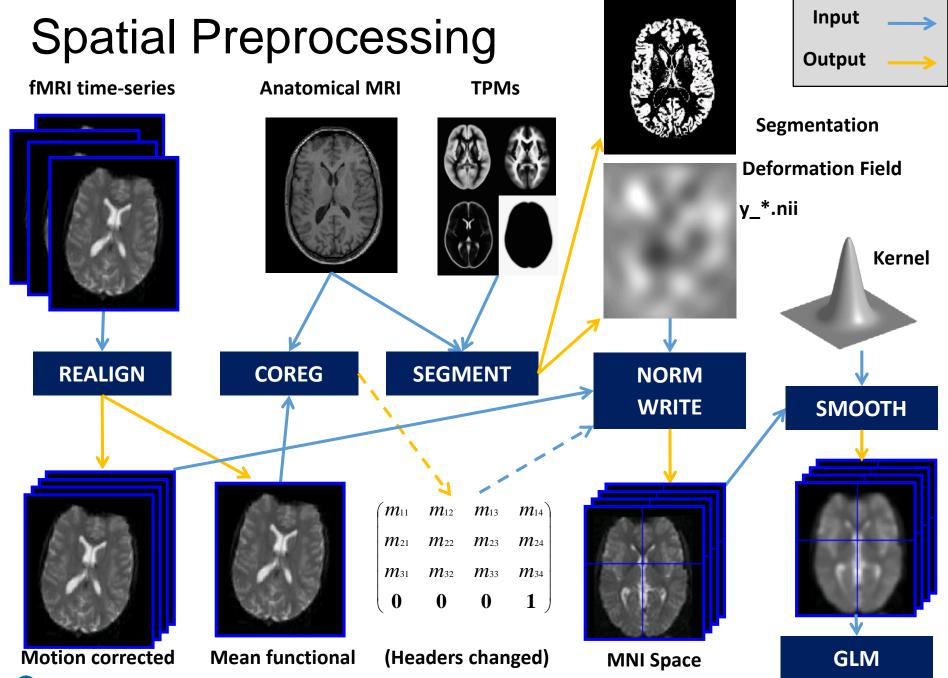


- Goal: Correct for different acquisition time of each slice within an image volume
- How: All voxel time series are aligned to acquisition time of 1 slice via Sincinterpolation of each voxel's time series



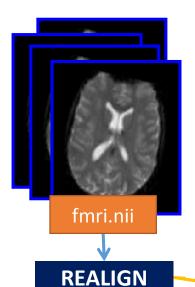


Slice-timing



Realignment

fMRI time-series

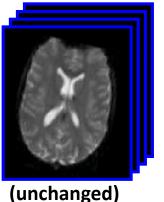


- Goal: Correct for subject motion between volumes
 by minimising mean-squared difference
- How: Rigid-body transformation
 - Note: Realignment improves if images are reoriented in advance (find the origin, change header, use check reg with the canonical image)

KEALIGN

fmri.nii

nii fmri.mat



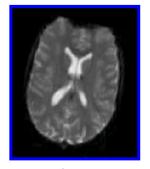
 $\begin{pmatrix} m_{11} & m_{12} & m_{13} & m_{14} \\ m_{21} & m_{22} & m_{23} & m_{24} \\ m_{31} & m_{32} & m_{33} & m_{34} \\ \mathbf{0} & \mathbf{0} & \mathbf{0} & \mathbf{1} \end{pmatrix}$

(Headers changed)

rp_fmri.txt

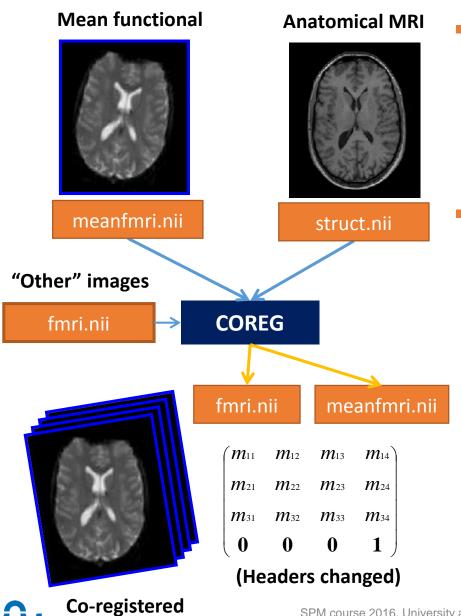
Realignment parameters





Mean functional

Co-registration



- Goal: Match geometry of functional and structural images from same subject
 - Structural = high-resolution, geometrically correct image for later normalisation
- How: Find affine transformation

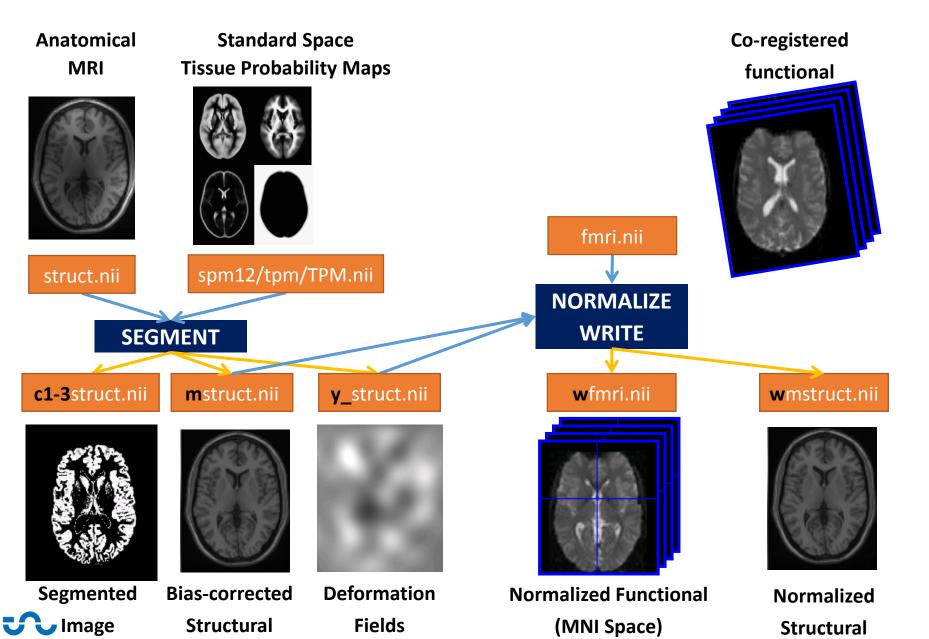
 (rotation/translation/shear/scaling) that
 maximizes mutual information

 (similarity) between both images
 - Note: The role of functional and structural image could be reversed in this operation

 *Reference = header unchanged

 *Source = header will be changed

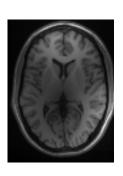
Normalisation: Unified Segmentation

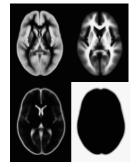


Normalisation I: Compute Segmentation/Deformation Fields

Anatomical MRI

Standard Space Tissue Probability Maps





struct.nii

spm12/tpm/TPM.nii

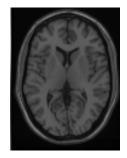
SEGMENT

c1-3struct.nii

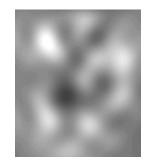
mstruct.nii

y_struct.nii





Structural



Segmented

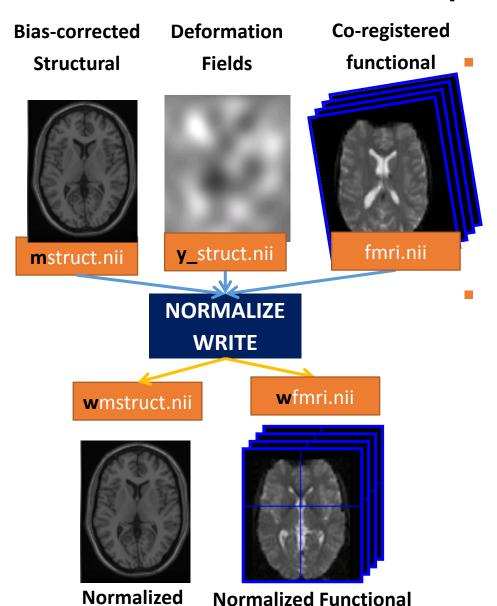
Image

Bias-corrected

Deformation Fields

- Goal: Match geometry of subject brain to standard space (for group studies)
 - Integrated with segmentation, since mapping individual tissue classes is more robust
- How: Find non-linear transformation (deformation field) that makes tissue class distribution in structural image most plausible
 - Assuming coil inhomogeneity (bias), and deformations of reasonable anatomy
 - Note: uses a Bayesian maximum a posteriori estimation, where standard space tissue probability maps (TPMs) are the priors

Normalisation II: Warp via Write



(MNI Space)

Goal: Write out functional/structural image in standard space for multi-subject statistical analysis

- to report findings in common anatomical space (e.g. MNI)
- How: Applies estimated deformation fields from Unified Segmentation to all functional and structural data
 - Deformation fields have a displacement vector for each image voxel that tells where it should be moved to in standard space

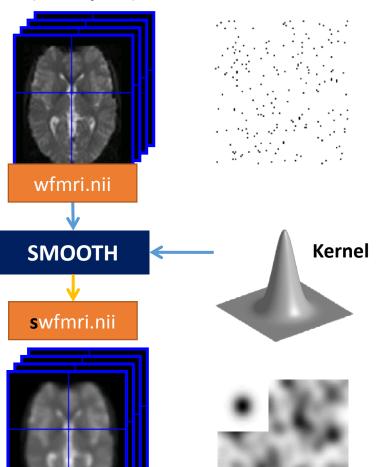
Structural

Smoothing

Input ---> Output --->

Normalized Functional

(MNI Space)



- Goal: Increase sensitivity by reducing thermal noise and inter-subject variability in functional images
 - Plus a couple of more sophisticated reasons,
 e.g. matched-filter theorem, smoothness of
 residual random field for FWE-correction
- How: Convolution ("Blurring") with a 3D Gaussian kernel
 - Each voxel effectively becomes a weighted average of its surroundings (interpolation)
 - Typical full width at half maximum: 2-3 voxel



Smoothed Images

SPM Image File Prefixes xfmri.nii/mat

| Prefix | Meaning | Typicallly applied to |
|--------|--|-----------------------|
| a | Slice-timing corrected | functional |
| m | Bias-field corrected (modulated) | structural |
| mean | Mean of time-series | functional |
| r | Re-sliced (change image matrix, reset hdr) | both |
| S | Smoothed | functional |
| u | Unwarped (during realign/FieldMap Tool) | functional |
| У_ | Deformation field | structural |
| W | Normalized (warped with deformation field) | both |



SPM File Operations in Matlab Command Window

| Operation | Matlab/SPM command |
|-------------------------------|--|
| Retrieve multiple file names | <pre>fNames = spm_select('FPList', pwd, '^sM.*\.img\$');</pre> |
| Plot Image(s) with SPM | spm_check_registration(fNames) |
| Load image header(s) | hdr = spm_vol(fNames); |
| Load Image Matrix | <pre>X = spm_read_vols(hdr);</pre> |
| Inspect Batch in Batch Editor | <pre>spm_jobman('interactive', matlabbatch);</pre> |
| Run Batch from command line | <pre>spm_jobman('initcfg'); %1st time spm_jobman('run',matlabbatch);</pre> |

