

# Classical (frequentist) inference

## Methods & models for fMRI data analysis

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With many thanks for slides & images to:  
FIL Methods group



Translational Neuromodeling Unit



**Universität  
Zürich**<sup>UZH</sup>

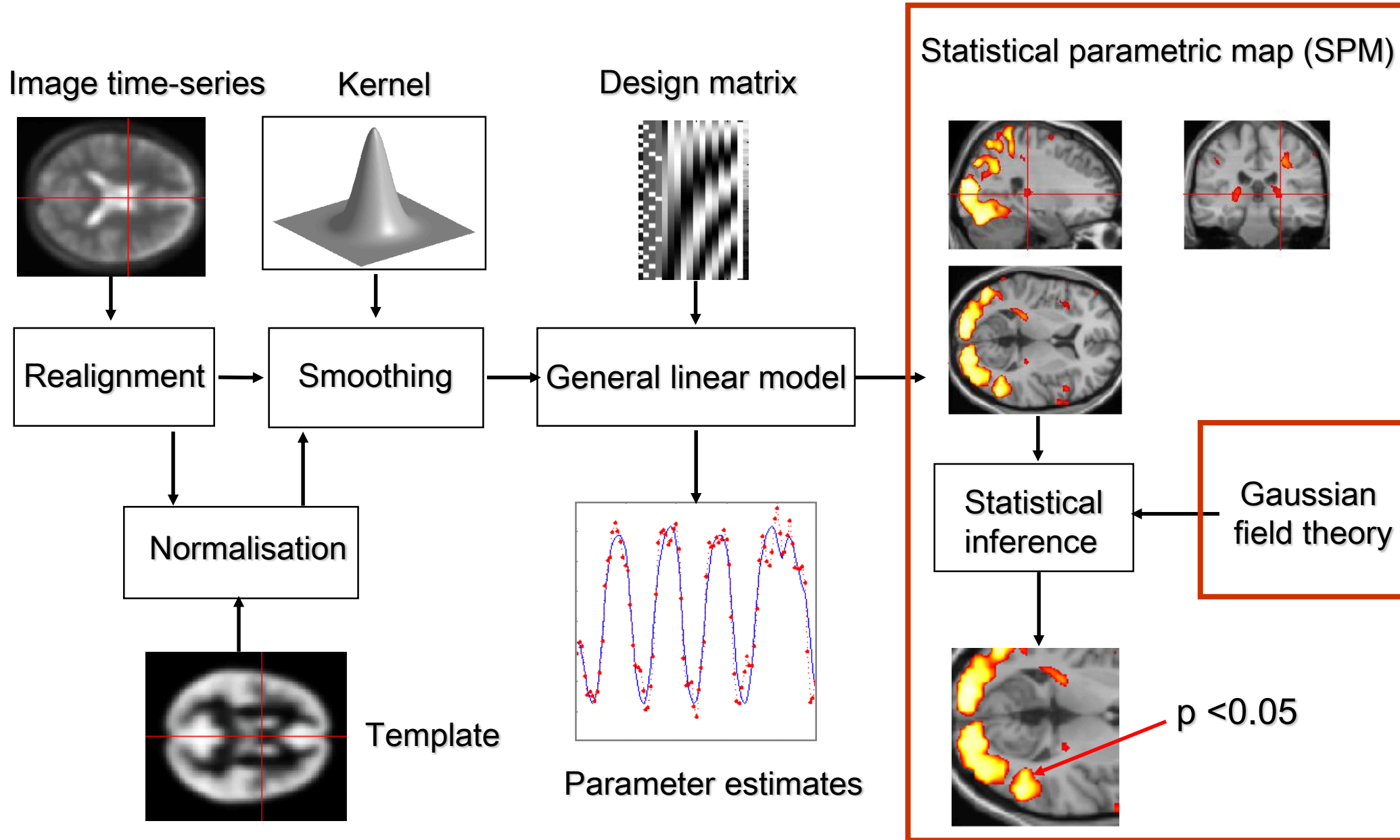


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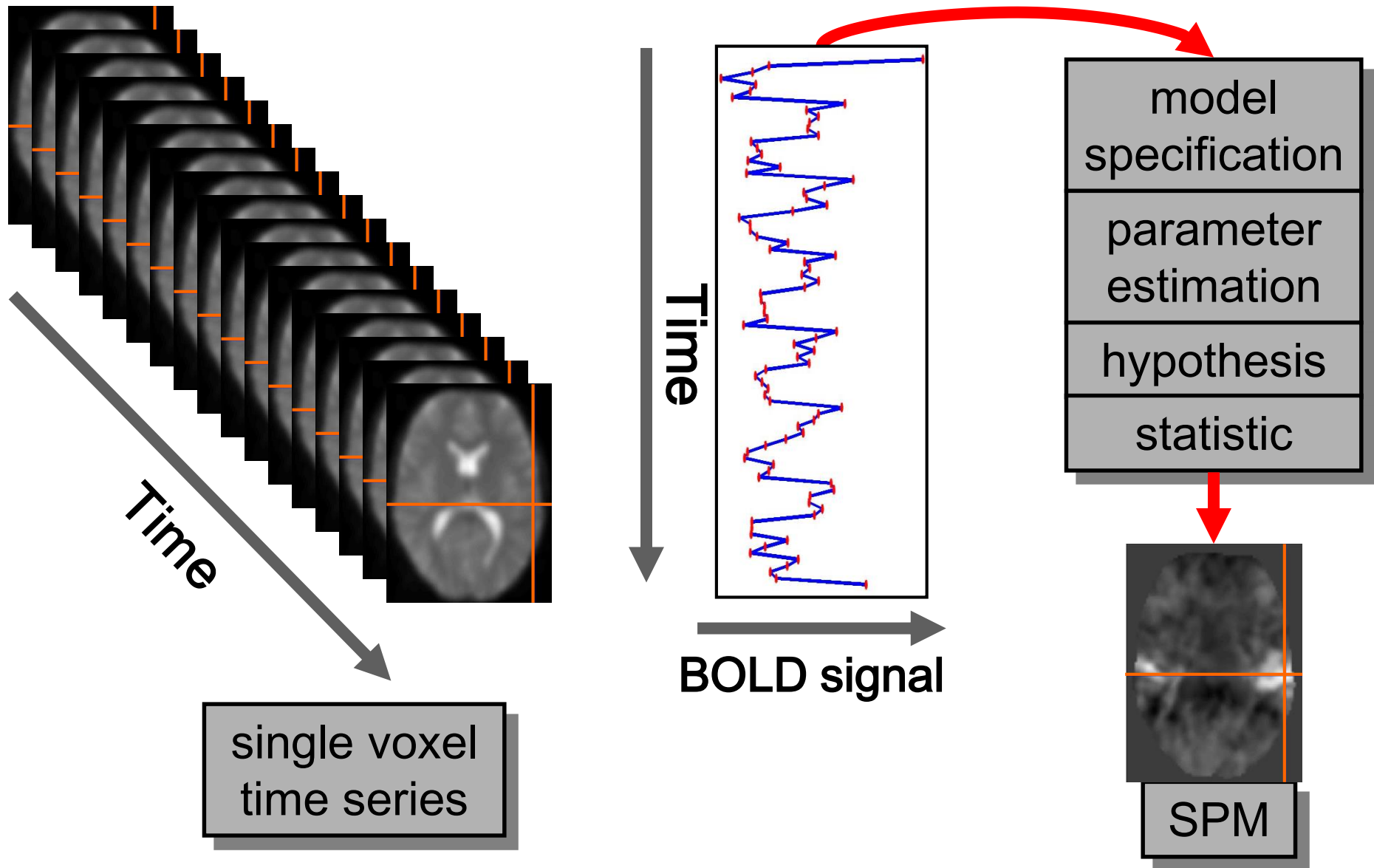
# Overview

- A recap of model specification and parameter estimation
- Hypothesis testing
- Contrasts and estimability
  - $T$ -tests
  - $F$ -tests
- Design orthogonality

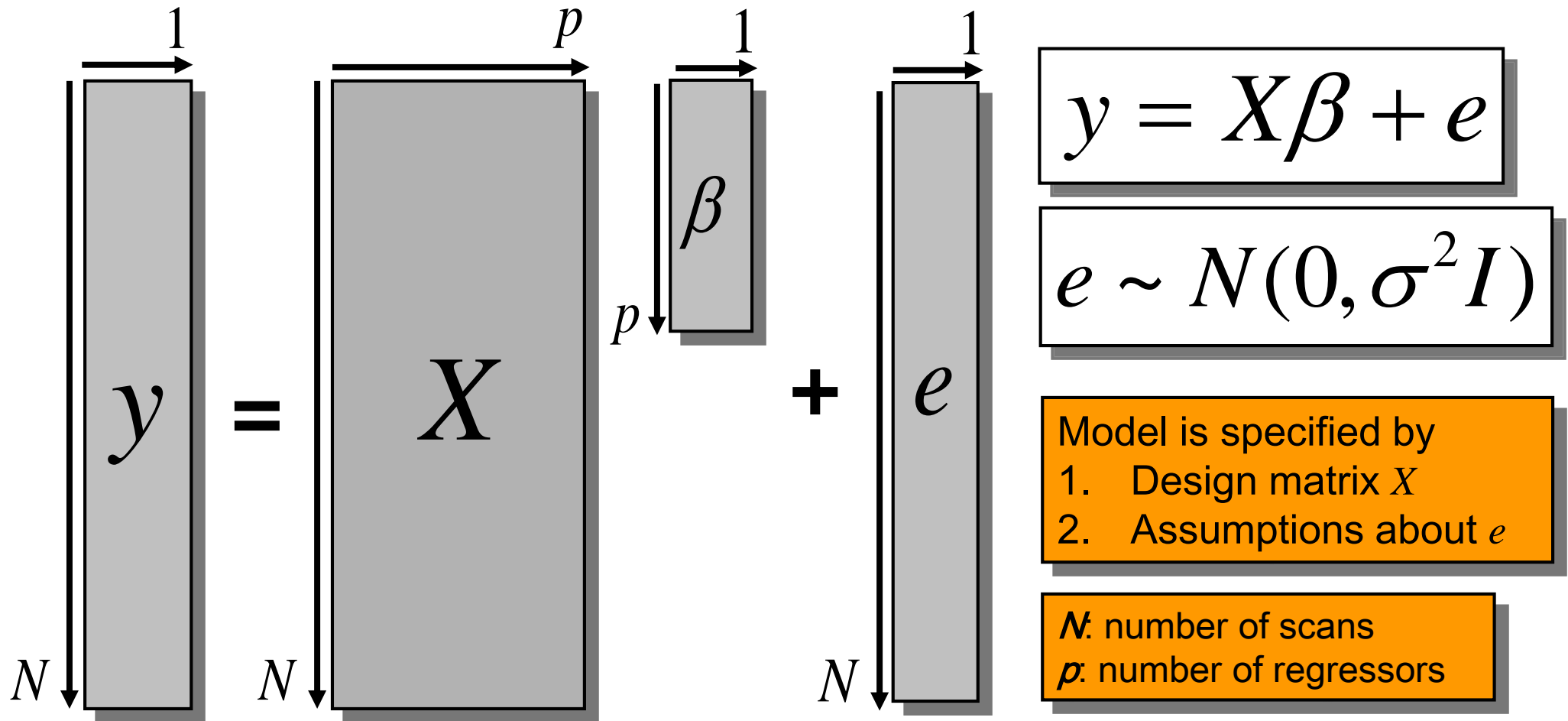
# Overview of SPM



# Voxel-wise time series analysis

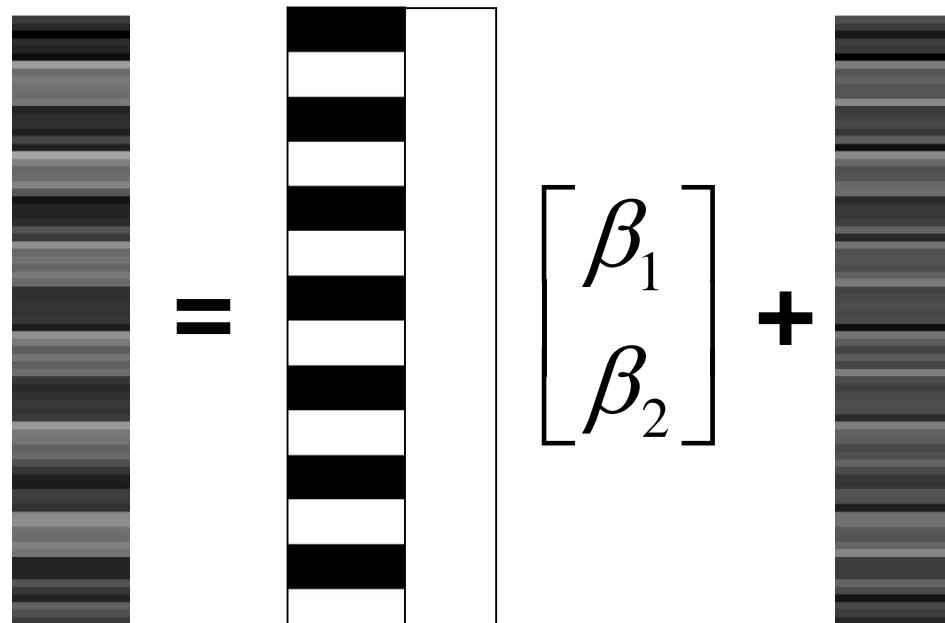


# Mass-univariate analysis: voxel-wise GLM



The design matrix embodies all available knowledge about experimentally controlled factors and potential confounds.

# Parameter estimation



$y = X \begin{bmatrix} \beta_1 \\ \beta_2 \end{bmatrix} + e$

$y$        $X$        $e$

$$y = X\beta + e$$

Objective:  
estimate parameters  
to minimize

$$\sum_{t=1}^N e_t^2$$



Ordinary least squares  
estimation (OLS)  
(assuming i.i.d. error):

$$\hat{\beta} = (X^T X)^{-1} X^T y$$

# OLS parameter estimation

The Ordinary Least Squares (OLS) estimators are:

$$\hat{\beta} = (X^T X)^{-1} X^T y$$

These estimators minimise

$$\sum e_t^2 = e^T e$$

. They are found solving either

$$\frac{\partial(\sum e_t^2)}{\partial \hat{\beta}_t} = 0$$

or

$$X^T e = 0$$

Under i.i.d. assumptions, the OLS estimates correspond to ML estimates:

$$e \sim N(0, \sigma^2 I) \longrightarrow Y \sim N(X\beta, \sigma^2 I)$$

$$\hat{\sigma}^2 = \frac{\hat{e}^T \hat{e}}{N - p}$$

$$\hat{\beta} \sim N(\beta, \sigma^2 (X^T X)^{-1})$$

NB: precision of our estimates  
depends on design matrix!

# Maximum likelihood (ML) estimation

probability density function ( $\theta$  fixed!)

$$y \mapsto f(y | \theta)$$

likelihood function ( $y$  fixed!)

$$\theta \mapsto f(y | \theta)$$

$$\theta \mapsto L(\theta | y)$$

$$L(\theta | y) = f(y | \theta)$$

ML estimator

$$\hat{\theta} = \arg \max_{\theta} L(\theta | y)$$

For  $\text{cov}(e) = \sigma^2 I$ , the ML estimator is equivalent to the OLS estimator:

$$\hat{\beta} = (X^T X)^{-1} X^T y$$

OLS

For  $\text{cov}(e) = \sigma^2 V$ , the ML estimator is equivalent to a weighted least squares (WLS) estimate (with  $W = V^{-1/2}$ ):

$$\hat{\beta} = (X^T W X)^{-1} X^T W y$$

WLS

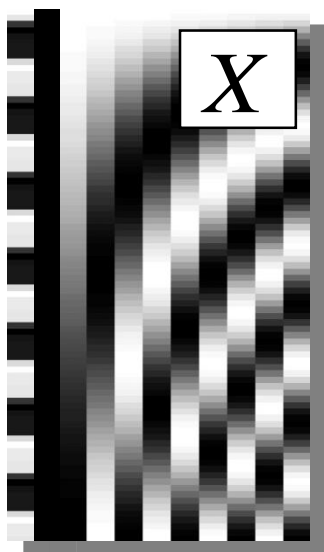


# Bonus material: t-statistic based on ML estimates in SPM

$$Wy = WX\beta + We$$

$$\hat{\beta} = (WX)^+ Wy$$

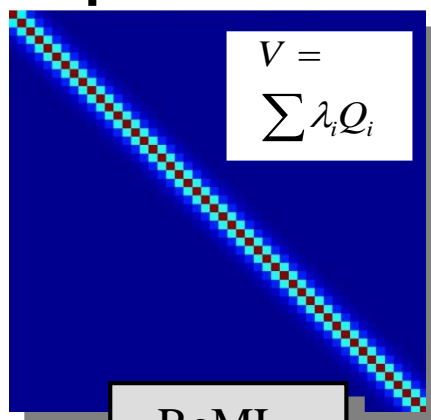
$$c = 10000000000$$



$$t = \frac{c^T \hat{\beta}}{\hat{std}(c^T \hat{\beta})}$$

$$W = V^{-1/2}$$

$$\sigma^2 V = Cov(e)$$



ReML-  
estimates

$$\hat{std}(c^T \hat{\beta}) = \sqrt{\hat{\sigma}^2 c^T (WX)^+ (WX)^{+T} c}$$

$$\hat{\sigma}^2 = \frac{\sum (Wy - WX\hat{\beta})^2}{tr(R)}$$

$$R = I - WX(WX)^+$$

For brevity:

$$(WX)^+ = (X^T W X)^{-1} X^T$$

# Statistic

- A **statistic** is the result of applying a mathematical function to a **sample** (set of data).
- More formally, a **statistic** is a function of a sample where the function itself is independent of the sample's distribution.  
(The term is used both for the function and for the value of the function on a given sample.)
- A statistic is distinct from an unknown statistical **parameter**, which is a population property and can only be estimated approximately from a sample.
- A statistic used to estimate a parameter is called an **estimator**.  
For example, the sample mean is a statistic and an estimator for the population mean, which is a parameter.

# Hypothesis testing

To test an hypothesis, we construct a “test statistic”.

- **“Null hypothesis”**  $H_0 = \text{“there is no effect”} \Rightarrow c^T \beta = 0$

This is what we want to disprove.

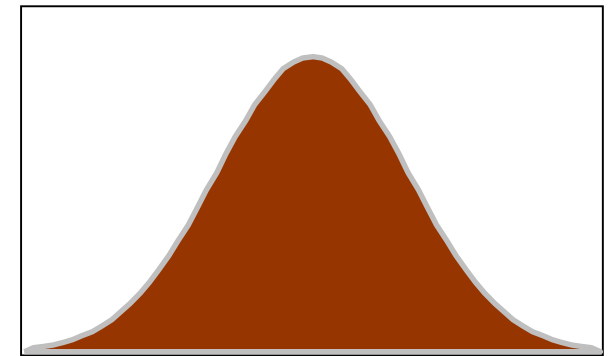
$\Rightarrow$  The “alternative hypothesis”  $H_1$  represents the outcome of interest.

- **The test statistic T**

The test statistic summarises the evidence for  $H_0$ .

Typically, the test statistic is small in magnitude when  $H_0$  is true and large when  $H_0$  is false.

$\Rightarrow$  We need to know the distribution of T under the null hypothesis.



Null Distribution of T

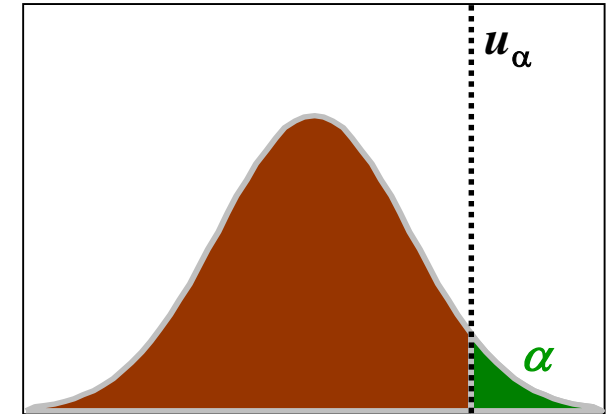
# Hypothesis testing

- **Type I Error  $\alpha$ :**

Acceptable *false positive rate*  $\alpha$ .

Threshold  $u_\alpha$  controls the false positive rate

$$\alpha = p(T > u_\alpha \mid H_0)$$



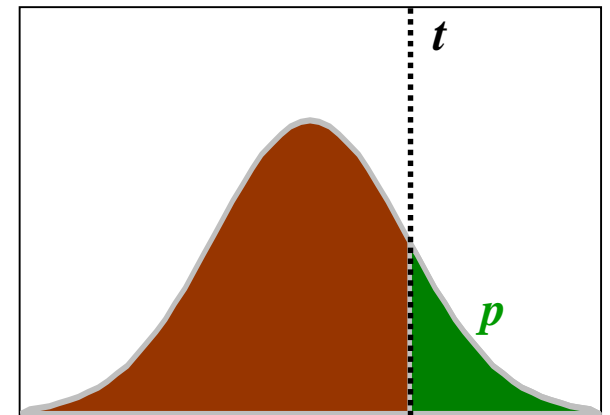
Null Distribution of T

- **Observation of test statistic  $t$ , a realisation of  $T$ :**

A  $p$ -value summarises evidence against  $H_0$ .

This is the probability of observing  $t$ , or a more extreme value, under the null hypothesis:

$$p(T \geq t \mid H_0)$$



Null Distribution of T

- **The conclusion about the hypothesis:**

We reject  $H_0$  in favour of  $H_1$  if  $t > u_\alpha$

# Types of error

Actual condition			
		$H_0$ true	$H_0$ false
Test result	Reject $H_0$	<b>False positive (FP)</b> <b>Type I error <math>\alpha</math></b>	<b>True positive (TP)</b>
	Failure to reject $H_0$	<b>True negative (TN)</b>	<b>False negative (FN)</b> <b>Type II error <math>\beta</math></b>
		<b>specificity: <math>1-\alpha</math></b> = $TN / (TN + FP)$ = proportion of actual negatives which are correctly identified	<b>sensitivity (power): <math>1-\beta</math></b> = $TP / (TP + FN)$ = proportion of actual positives which are correctly identified

**One cannot accept the null hypothesis  
(one can only fail to reject it)**



**Absence of evidence is not evidence of absence!**

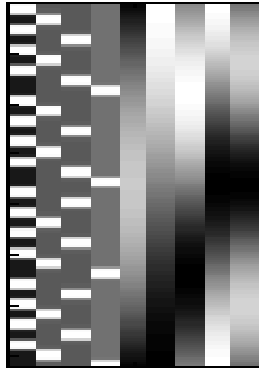
If we do not reject  $H_0$ , then all we can say is that there is not enough evidence in the data to reject  $H_0$ . This does not mean that we can accept  $H_0$ .

**What does this mean for neuroimaging results based on classical statistics?**

A failure to find an “activation” in a particular area does not mean we can conclude that this area is not involved in the process of interest.

# Contrasts

- We are usually not interested in the whole  $\beta$  vector.
- A contrast  $c^T \beta$  selects a specific effect of interest:
  - $\Rightarrow$  a contrast vector  $c$  is a vector of length  $p$
  - $\Rightarrow c^T \beta$  is a linear combination of regression coefficients  $\beta$



$$c^T = [1 \ 0 \ 0 \ 0 \ 0 \ \dots]$$

$$c^T \beta = 1\beta_1 + 0\beta_2 + 0\beta_3 + 0\beta_4 + 0\beta_5 + \dots$$

$$c^T = [0 \ -1 \ 1 \ 0 \ 0 \ \dots]$$

$$c^T \beta = 0\beta_1 + -1\beta_2 + 1\beta_3 + 0\beta_4 + 0\beta_5 + \dots$$

- Under i.i.d assumptions:

$$c^T \hat{\beta} \sim N(c^T \beta, \sigma^2 c^T (X^T X)^{-1} c)$$

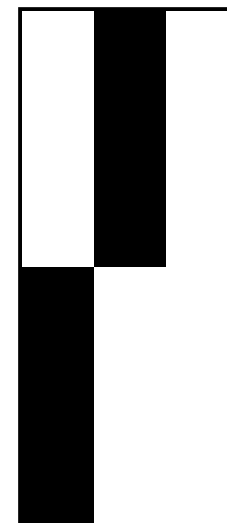
NB: the precision of our estimates depends on design matrix and the chosen contrast !

# Bonus material: Estimability of parameters

- If  $X$  is not of **full rank** then different parameters can give identical predictions, i.e.  $X\beta_1 = X\beta_2$  with  $\beta_1 \neq \beta_2$ .
- The parameters are therefore ‘non-unique’, ‘non-identifiable’ or ‘**non-estimable**’.
- For such models,  $X^T X$  is not invertible so we must resort to generalised inverses (SPM uses the Moore-Penrose **pseudo-inverse**).
- This gives a parameter vector that has the smallest norm of all possible solutions.
- However, even when parameters are non-estimable, certain contrasts may well be!

One-way ANOVA  
(unpaired two-sample  $t$ -test)

1	0	1
1	0	1
1	0	1
1	0	1
0	1	1
0	1	1
0	1	1
0	1	1

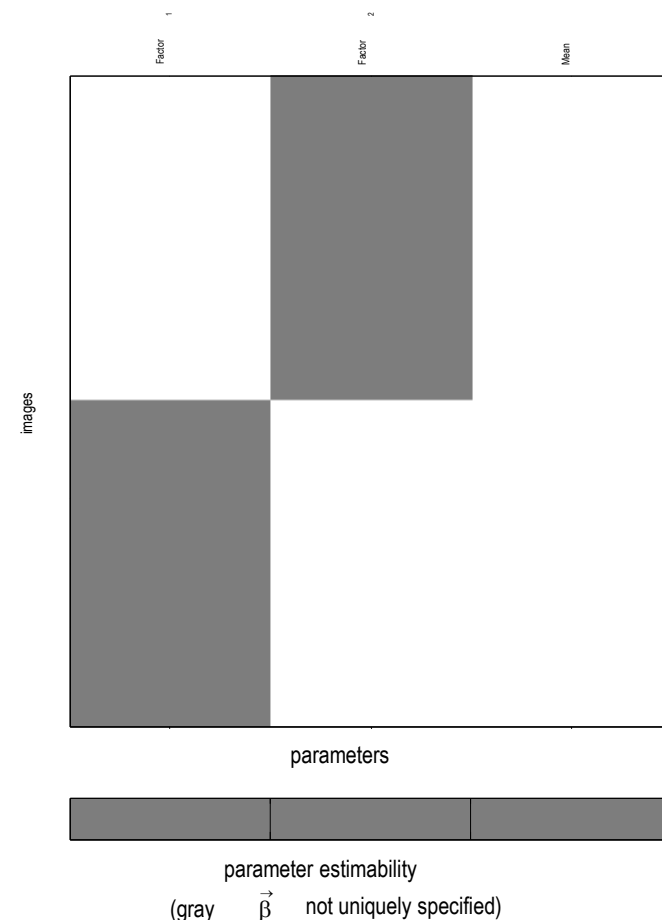


Rank( $X$ )=2



# Bonus material: Estimability of parameters

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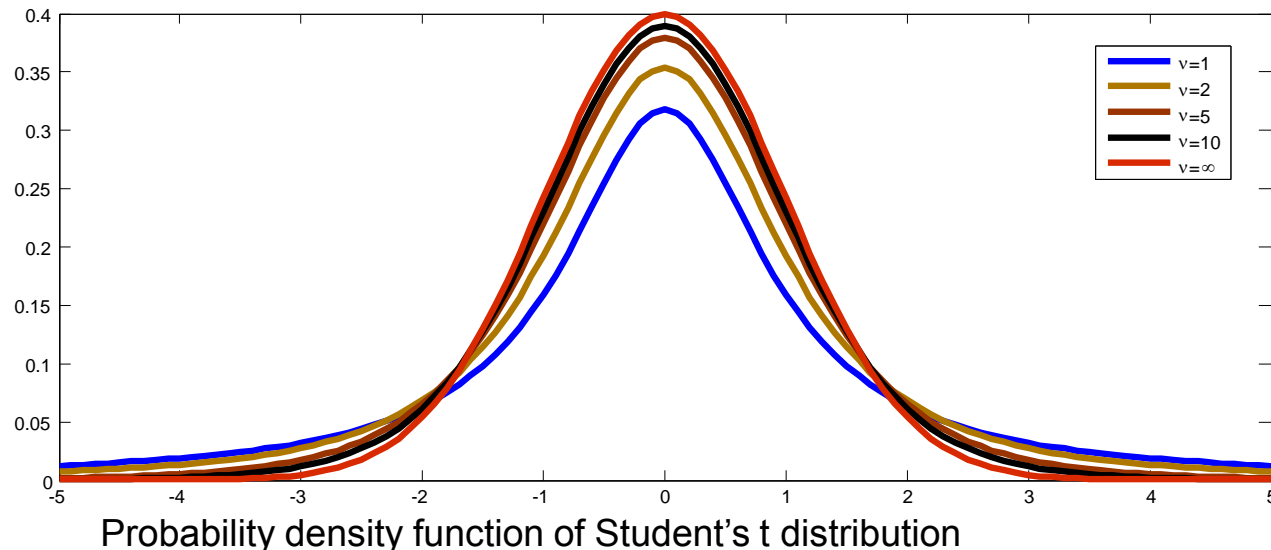


## Bonus material: Estimability of contrasts

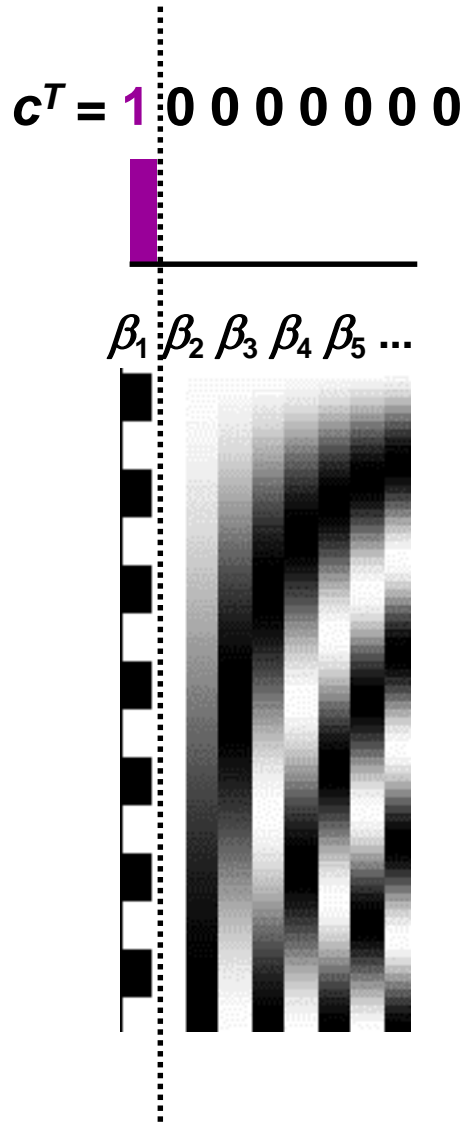
- Linear dependency: there is one contrast vector  $q$  for which  $Xq = 0$ .
- Thus:  $y = X\beta + Xq + e = X(\beta + q) + e$
- So if we test  $c^T\beta$  we also test  $c^T(\beta + q)$ , thus an estimable contrast has to satisfy  $c^Tq = 0$ .
- In the above ANOVA example (unpaired t-test), any contrast that is orthogonal to  $[1 \ 1 \ -1]$  is estimable:  
[1 0 0], [0 1 0], [0 0 1] are not estimable.  
[1 0 1], [0 1 1], [1 -1 0], [0.5 0.5 1] are estimable.

# Student's t-distribution

- first described by William Sealy Gosset, a statistician at the Guinness brewery at Dublin
- t-statistic is a signal-to-noise measure:  $t = \text{effect} / \text{standard deviation}$
- t-distribution is an approximation to the normal distribution for small samples
- t-contrasts are simply linear combinations of the betas  
 $\Rightarrow$  the t-statistic does not depend on the scaling of the regressors or on the scaling of the contrast
- Unilateral test:  $H_0 : c^T \beta = 0$  vs.  $H_1 : c^T \beta > 0$



## t-contrasts – SPM{t}



### Question:

box-car amplitude  $> 0$  ?

$$H_1 = c^\top \beta > 0 ?$$

## Null hypothesis:

$$H_0: c^T \beta = 0$$

**Test statistic:**

***contrast of  
estimated  
parameters***

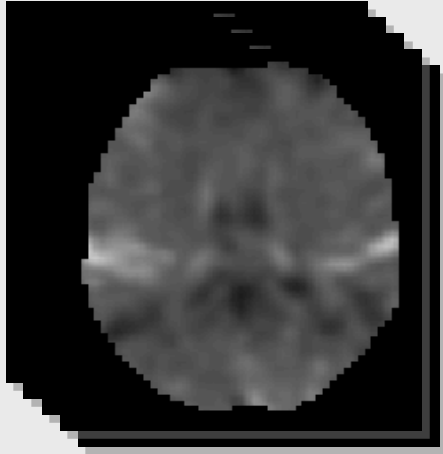
$$t = \frac{\text{variance estimate}}{\sqrt{\text{variance estimate}}}$$

$$p(y \mid c^T \hat{\beta} = 0)$$

$$t = \frac{c^T \hat{\beta}}{\hat{\sigma} \hat{d}(c^T \hat{\beta})} = \frac{c^T \hat{\beta}}{\sqrt{\hat{\sigma}^2 c^T (X^T X)^{-1} c}} \sim t_{N-p}$$

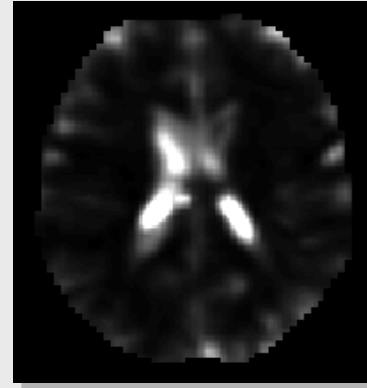
# t-contrasts in SPM

For a given contrast  $c$ :



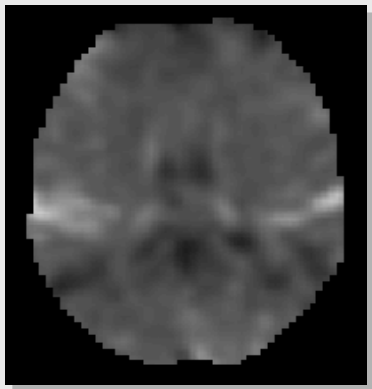
beta\_???? images

$$\hat{\beta} = (X^T X)^{-1} X^T y$$



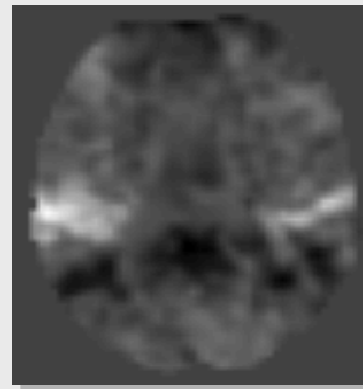
ResMS image

$$\hat{\sigma}^2 = \frac{\hat{e}^T \hat{e}}{N - p}$$



con\_???? image

$$c^T \hat{\beta}$$



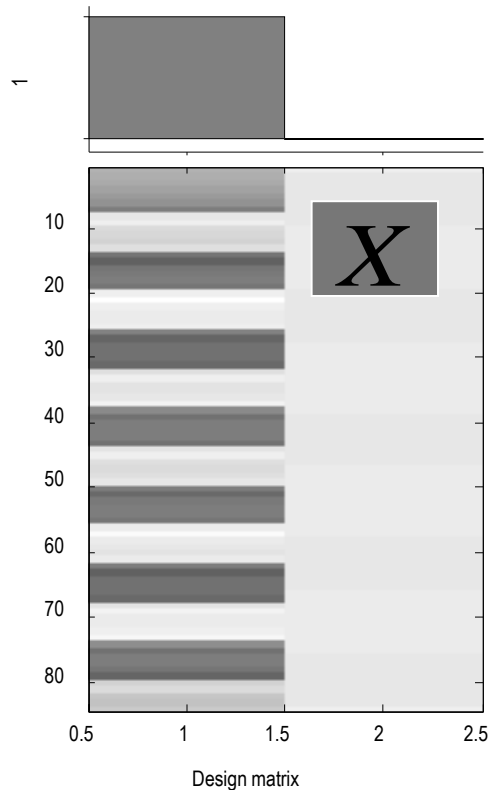
spmT\_???? image

SPM{ $t$ }

# t-contrast: a simple example

Passive word listening versus rest

$$c^T = [1 \quad 0]$$

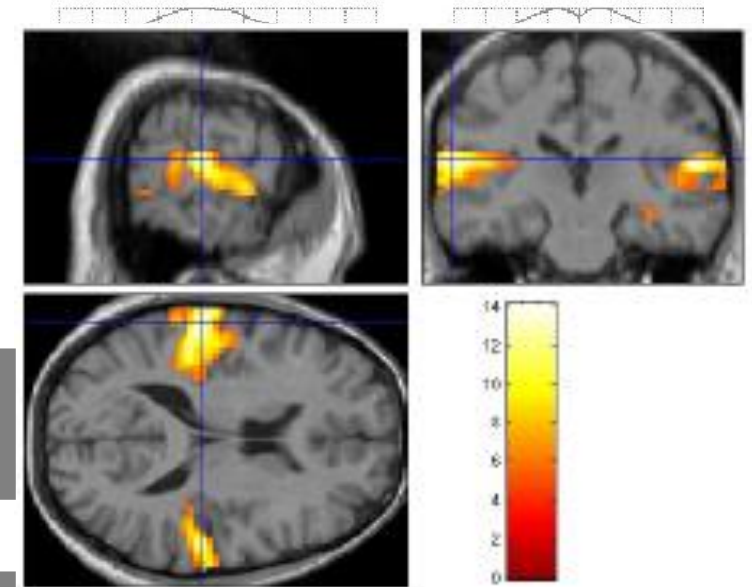


Q: activation during listening ?

Null hypothesis:  $\beta_1 = 0$

$$t = \frac{c^T \hat{\beta}}{Std(c^T \hat{\beta})}$$

$$p(y | c^T \hat{\beta} = 0)$$



SPMresults:  
Height threshold  $T = 3.2057$   $\{p < 0.001\}$

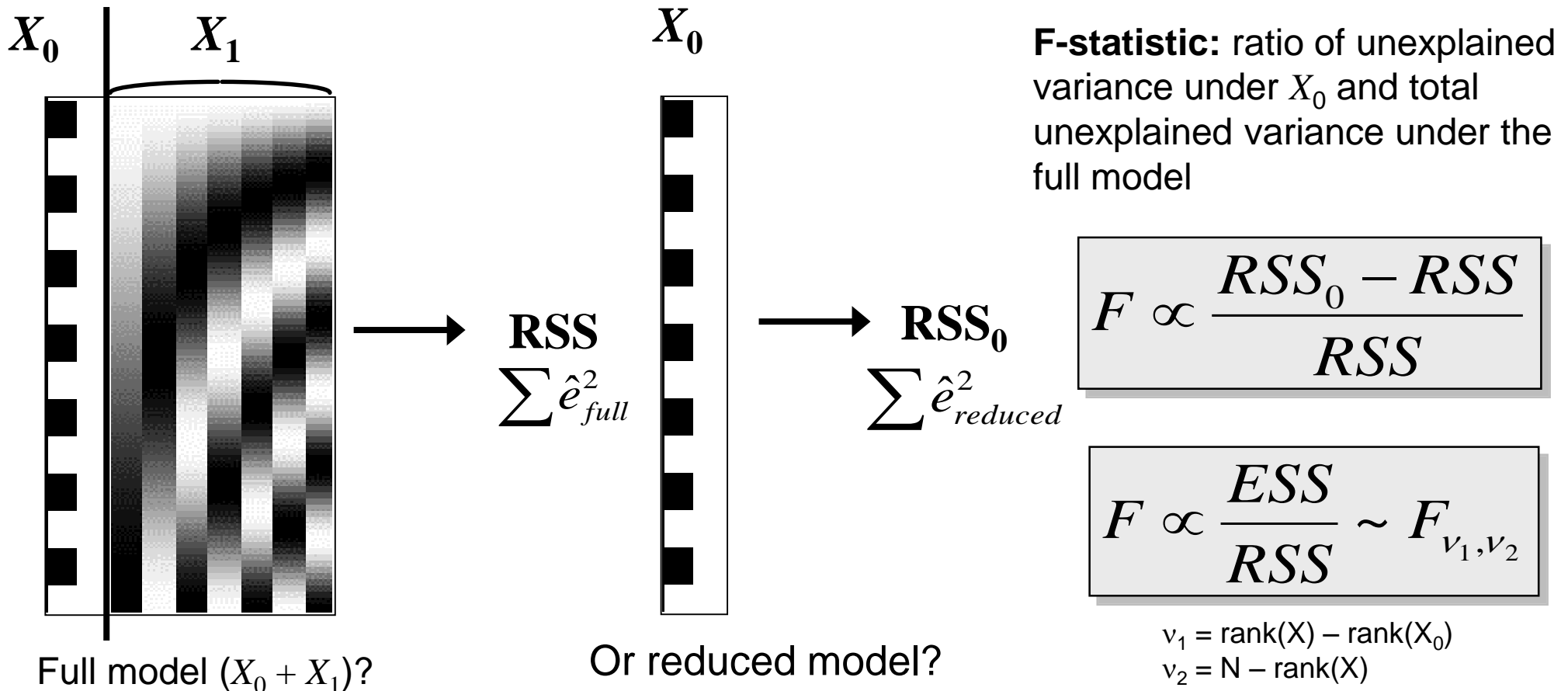
Statistics: *p-values adjusted for search volume*

set-level		cluster-level			voxel-level							
$p$	$c$	$p_{corrected}$	$k_E$	$p_{uncorrected}$	$p_{FWE-corr}$	$p_{FDR-corr}$	$T$	$(Z)$	$p_{uncorrected}$	mm	mm	mm
0.000	10	0.000	520	0.000	0.000	0.000	13.94	Inf	0.000	-63	-27	15
					0.000	0.000	12.04	Inf	0.000	-48	-33	12
					0.000	0.000	11.82	Inf	0.000	-66	-21	6
		0.000	426	0.000	0.000	0.000	13.72	Inf	0.000	57	-21	12
					0.000	0.000	12.29	Inf	0.000	63	-12	-3
					0.000	0.000	9.89	7.83	0.000	57	-39	6
		0.000	35	0.000	0.000	0.000	7.39	6.36	0.000	36	-30	-15
		0.000	9	0.000	0.000	0.000	6.84	5.99	0.000	51	0	48
		0.002	3	0.024	0.001	0.000	6.36	5.65	0.000	-63	-54	-3
		0.000	8	0.001	0.001	0.000	6.19	5.53	0.000	-30	-33	-18
		0.000	9	0.000	0.003	0.000	5.96	5.36	0.000	36	-27	9
		0.005	2	0.058	0.004	0.000	5.84	5.27	0.000	-45	42	9
		0.015	1	0.166	0.022	0.000	5.44	4.97	0.000	48	27	24
		0.015	1	0.166	0.036	0.000	5.32	4.87	0.000	36	-27	42

# F-test: the extra-sum-of-squares principle

Model comparison: Full vs. reduced model

**Null Hypothesis  $H_0$ :** True model is  $X_0$  (reduced model)



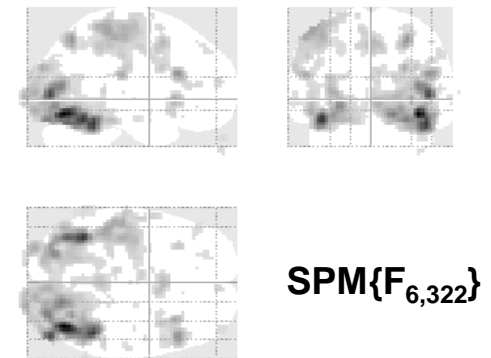
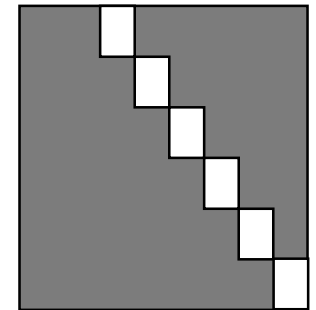
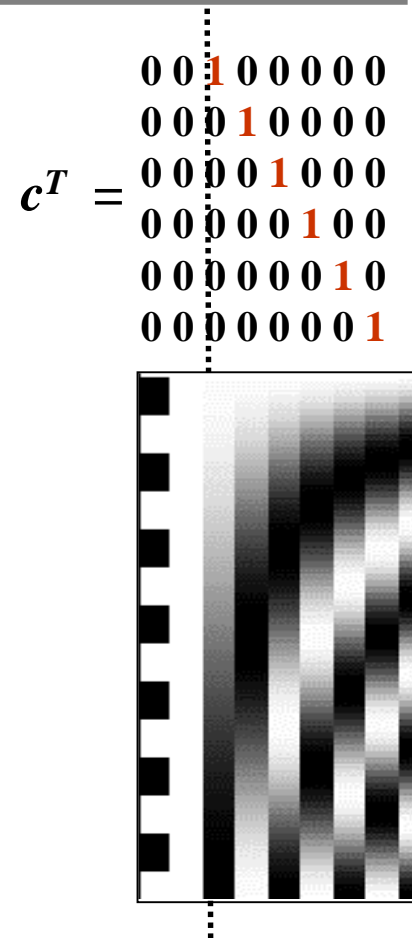
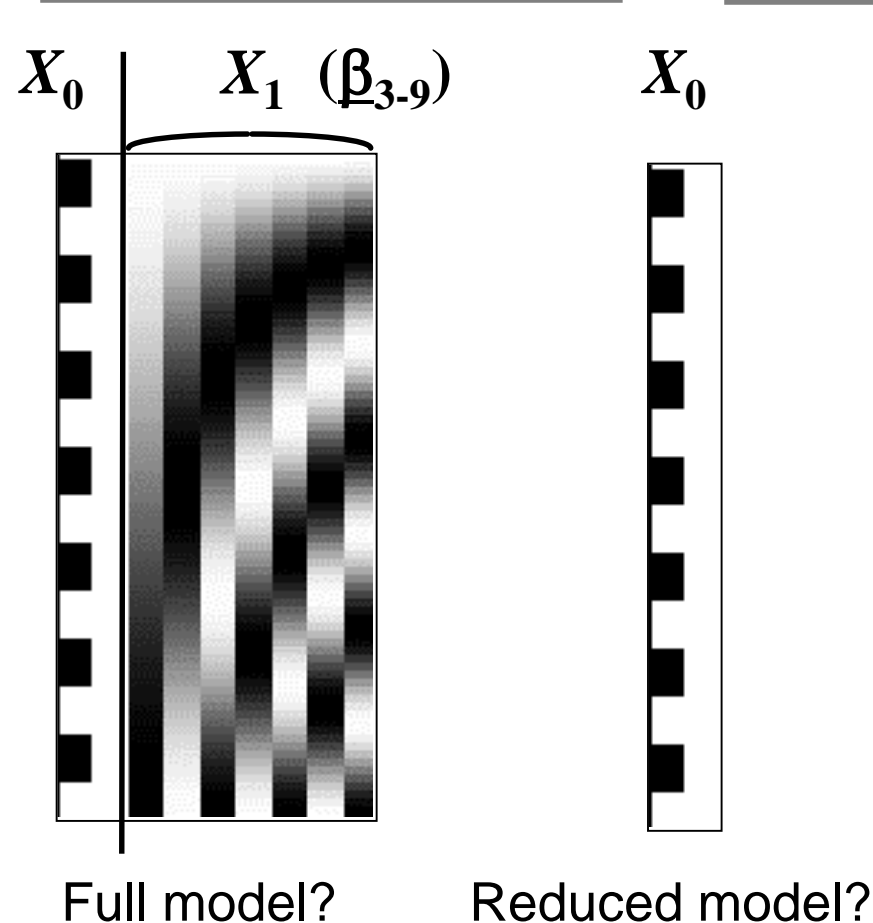
# F-test: multidimensional contrasts – SPM{F}

Tests multiple linear hypotheses:

$H_0$ : True model is  $X_0$

$H_0: \beta_3 = \beta_4 = \dots = \beta_9 = 0$

test  $H_0: c^T \beta = 0$  ?





# F-test: a few remarks

- F-tests can be viewed as testing for the additional variance explained by a larger model wrt. a simpler (nested) model  $\Rightarrow$  model comparison

- Hypotheses:

$$\begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & 0 \\ 0 & 0 & 1 & 0 \\ 0 & 0 & 0 & 0 \end{bmatrix}$$

**Null hypothesis  $H_0$ :**

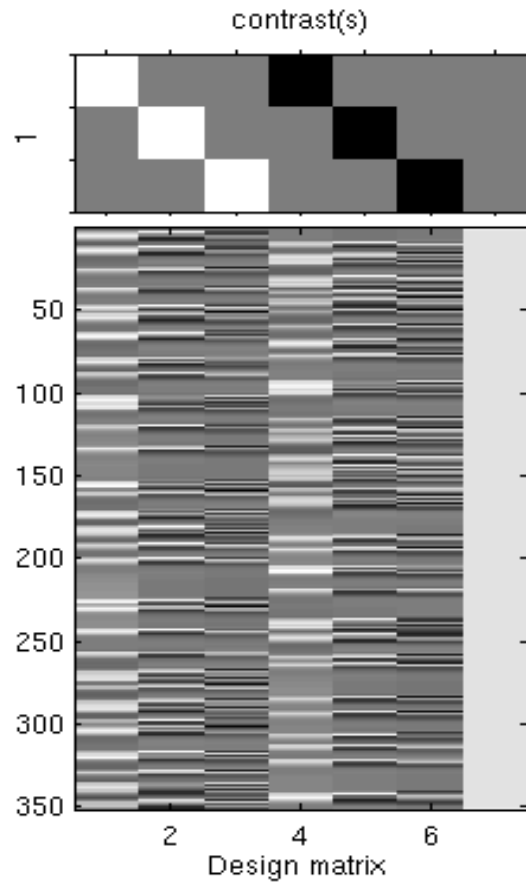
$$\beta_1 = \beta_2 = \dots = \beta_p = 0$$

**Alternative hypothesis  $H_1$ :**

At least one  $\beta_k \neq 0$

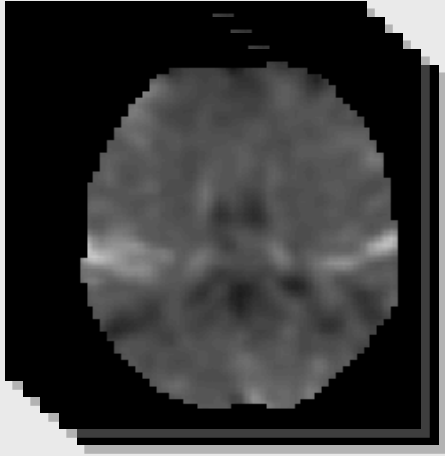
- F-tests are not directional:  
When testing a uni-dimensional contrast with an  $F$ -test, for example  $\beta_1 - \beta_2$ , the result will be the same as testing  $\beta_2 - \beta_1$ .

# Bonus material: Differential F-contrasts



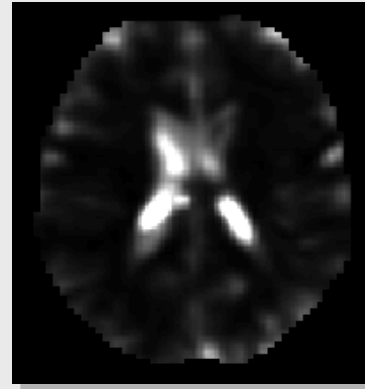
- equivalent to testing for effects that can be explained as a linear combination of the 3 differences
- useful when using informed basis functions and testing for overall shape differences in the HRF between two conditions

# F-contrast in SPM



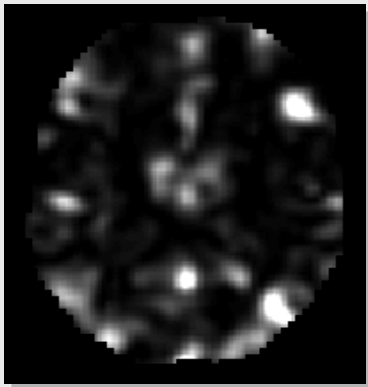
beta\_???? images

$$\hat{\beta} = (X^T X)^{-1} X^T y$$



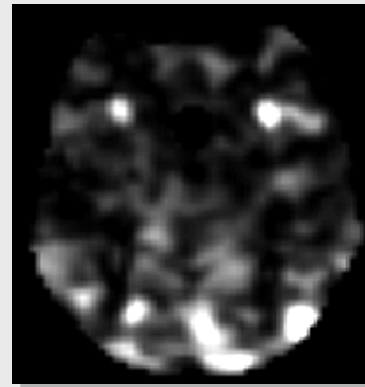
ResMS image

$$\hat{\sigma}^2 = \frac{\hat{e}^T \hat{e}}{N - p}$$



ess\_???? images

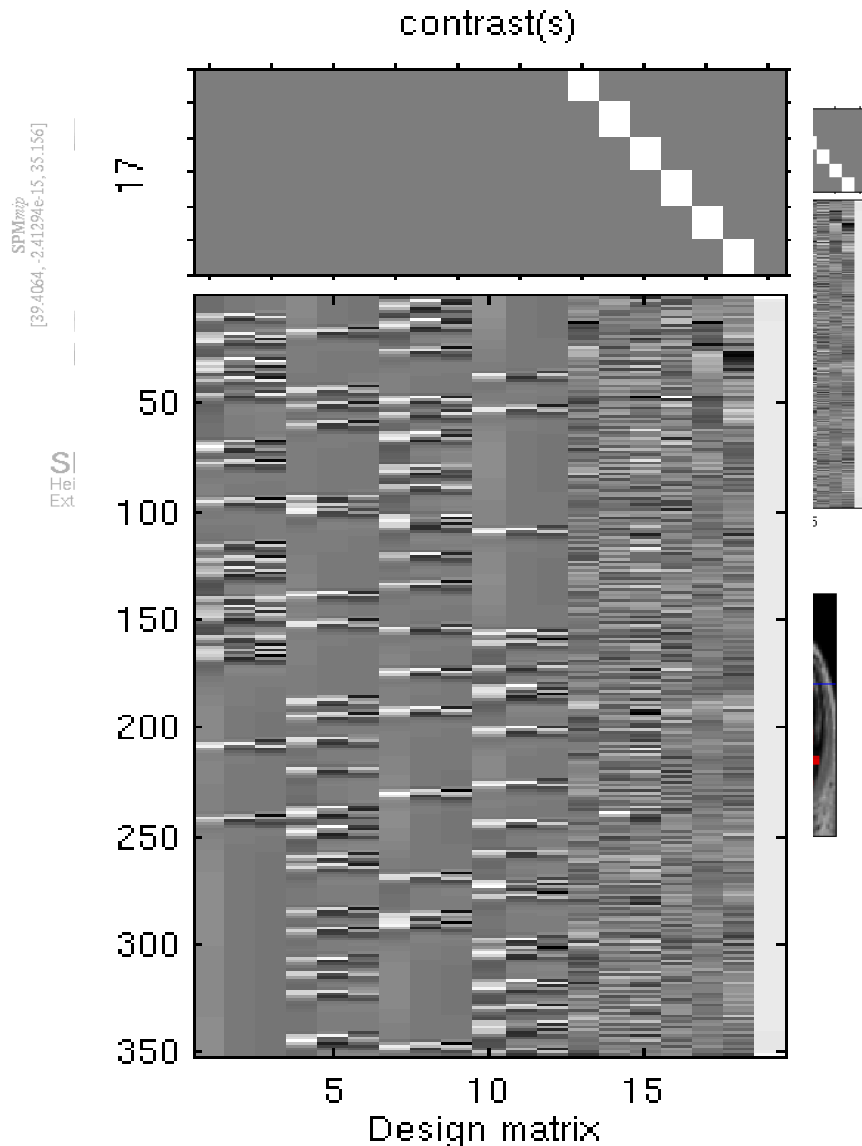
$$(RSS_0 - RSS)$$



spmF\_???? images

SPM{F}

# F-test example: movement related effects

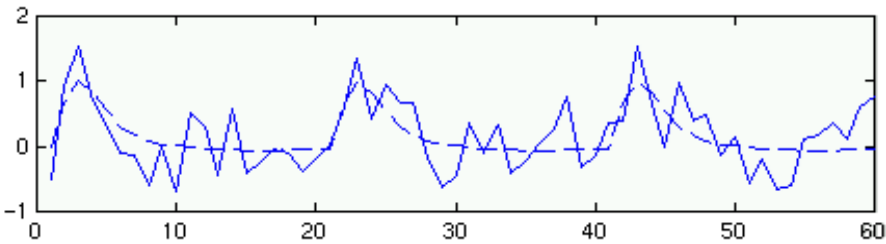


## To assess movement-related activation:

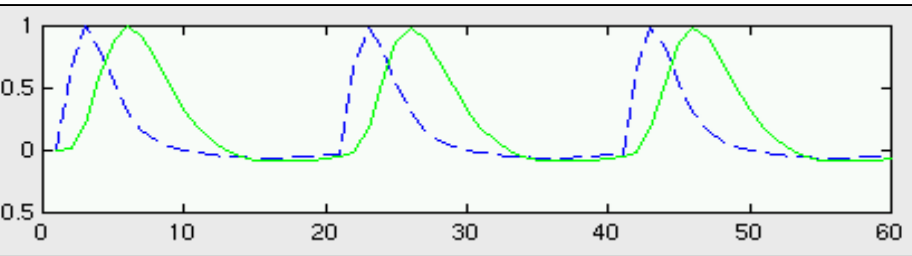
There is a lot of residual movement-related artifact in the data (despite spatial realignment), which tends to be concentrated near the boundaries of tissue types.

By including the realignment parameters in our design matrix, we can “regress out” linear components of subject movement, reducing the residual error, and hence improve our statistics for the effects of interest.

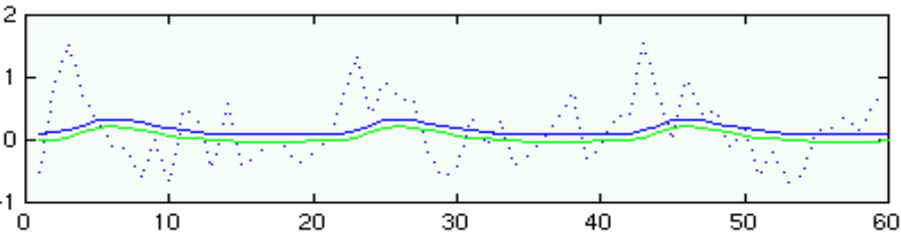
# Example: a suboptimal model



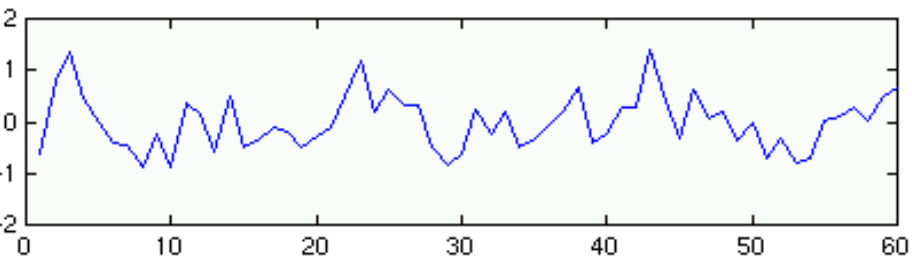
True signal (--) and observed signal



Model (green, peak at 6sec)  
TRUE signal (blue, peak at 3sec)



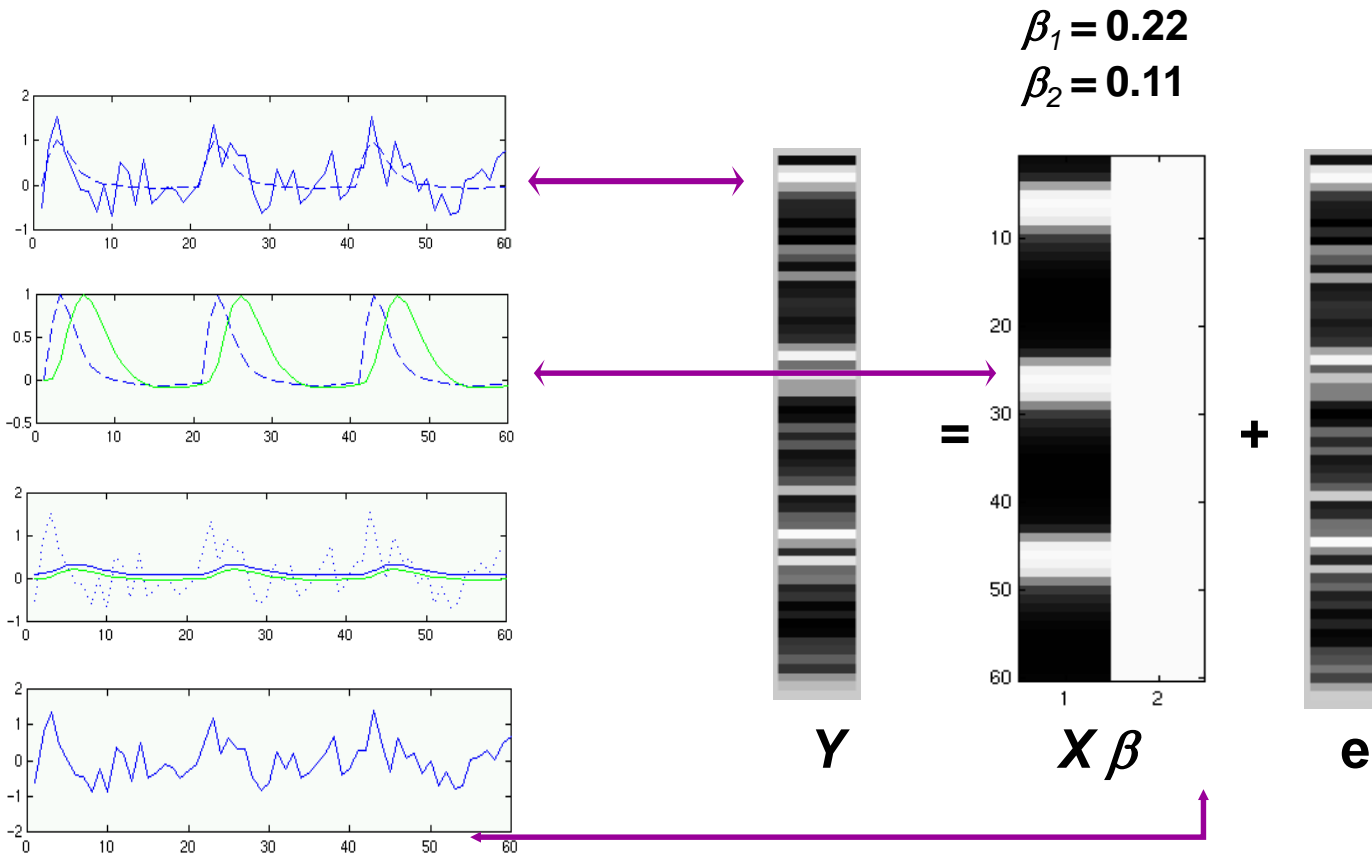
Fitting ( $\beta_1 = 0.2$ ,  $\beta_2$  (const.) = 0.11);  
(here: blue solid line = total fit)



Residuals (still contain some signal)

⇒ Test for the green regressor not significant

# Example: a suboptimal model

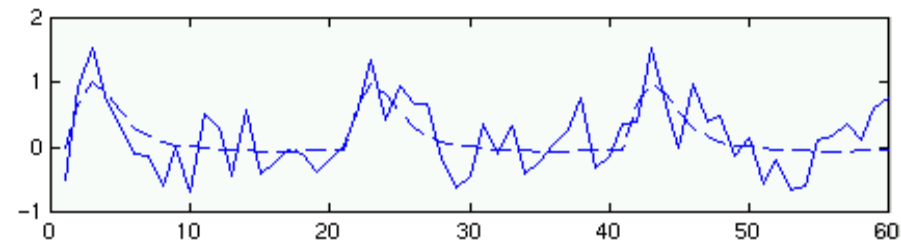


*Residual Var.* = 0.3

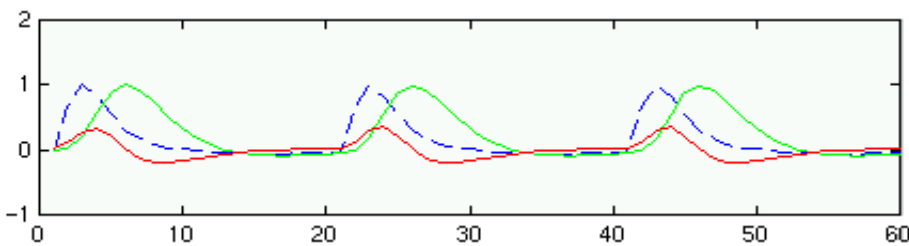
$p(Y/ b_1 = 0) \Rightarrow$   
 $p\text{-value} = 0.1$   
( $t$ -test)

$p(Y/ b_1 = 0) \Rightarrow$   
 $p\text{-value} = 0.2$   
( $F$ -test)

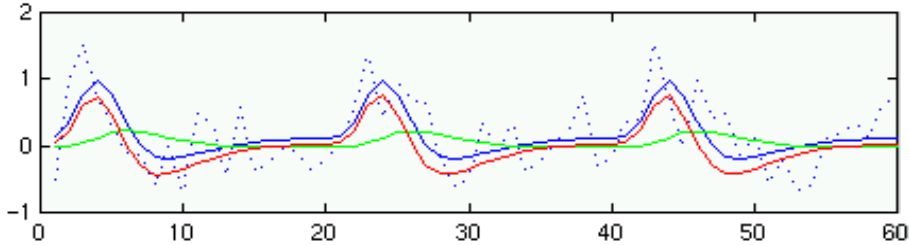
# A better model



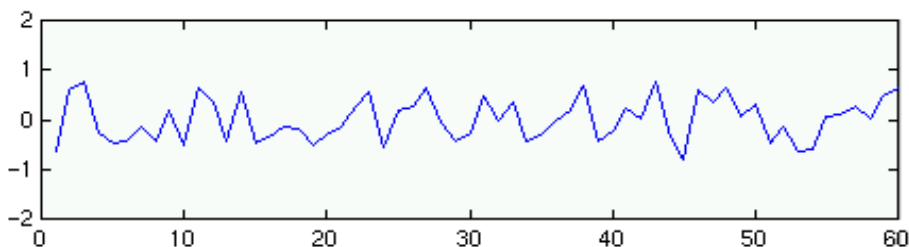
True signal + observed signal



Model (green and red)  
and true signal (blue ---)  
Red regressor: temporal derivative of  
the green regressor



Total fit (blue)  
and partial fit (green & red)  
Adjusted and fitted signal

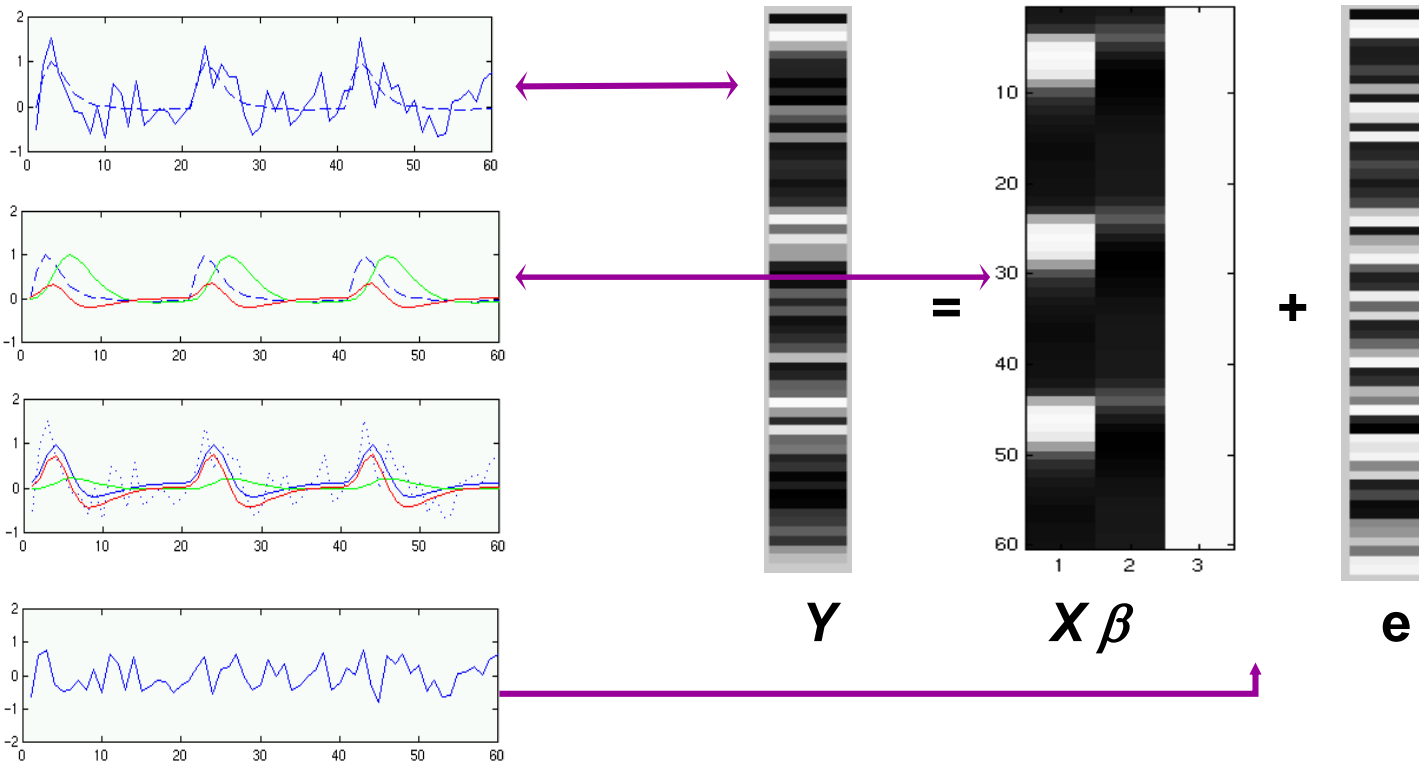


Residuals (less variance & structure)

- ⇒  $t$ -test of the green regressor almost significant
- ⇒  $F$ -test very significant
- ⇒  $t$ -test of the red regressor very significant

# A better model

$$\begin{aligned}\beta_1 &= 0.22 \\ \beta_2 &= 2.15 \\ \beta_3 &= 0.11\end{aligned}$$



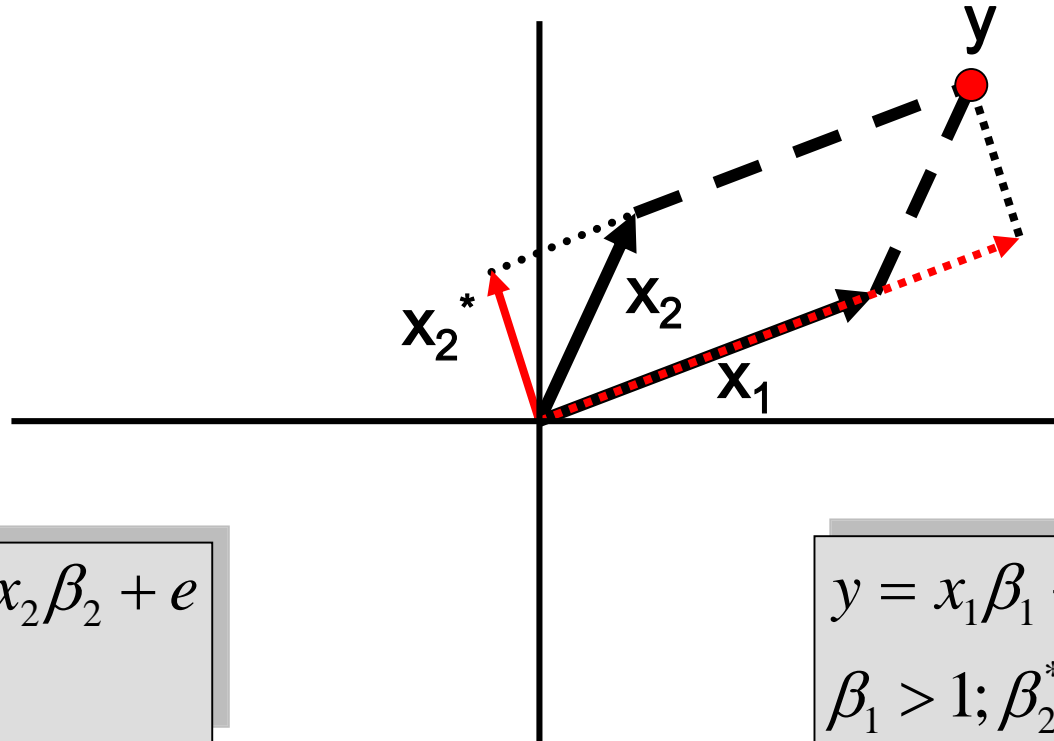
*Residual Var.* = 0.2

$$\begin{aligned}p(Y/ b_1 = 0) &\Rightarrow \\ p\text{-value} &= 0.07 \\ &\text{(t-test)}\end{aligned}$$

$$\begin{aligned}p(Y/ b_1 = 0, b_2 = 0) &\Rightarrow \\ p\text{-value} &= 0.000001 \\ &\text{(F-test)}\end{aligned}$$



# Recap from previous lecture: Correlation among regressors



$$y = x_1\beta_1 + x_2\beta_2 + e$$
$$\beta_1 = \beta_2 = 1$$

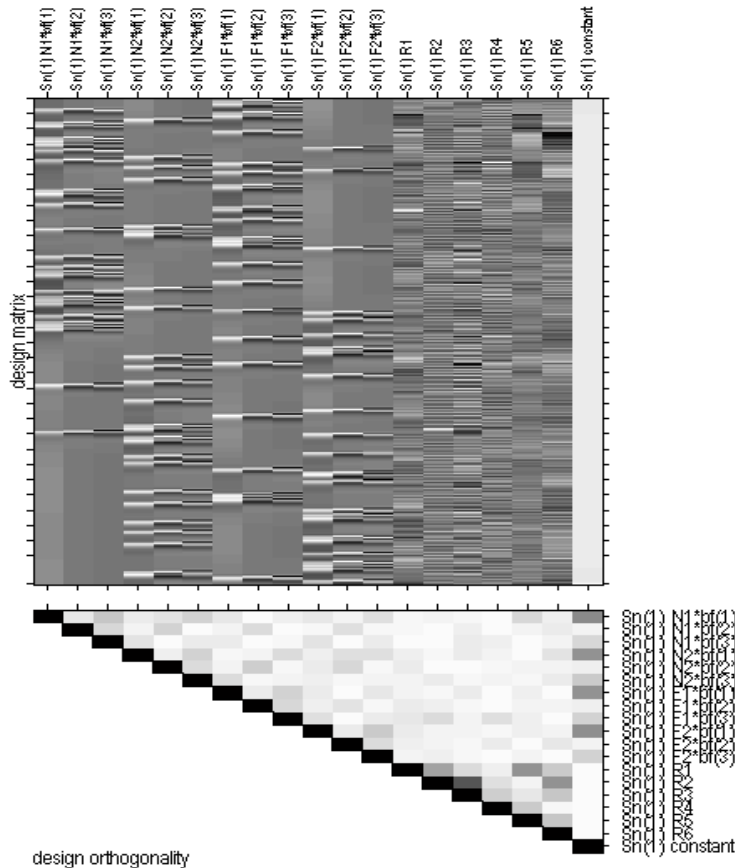
Correlated regressors =  
explained variance is shared  
between regressors

$$y = x_1\beta_1 + x_2^*\beta_2^* + e$$
$$\beta_1 > 1; \beta_2^* = 1$$

When  $x_2$  is orthogonalized with  
regard to  $x_1$ , only the parameter  
estimate for  $x_1$  changes, not that  
for  $x_2$ !

# Design orthogonality

## Statistical analysis: Design orthogonality



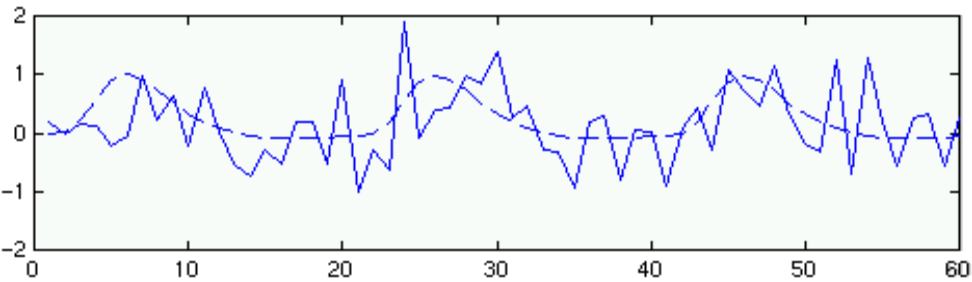
- For each pair of columns of the design matrix, the orthogonality matrix depicts the magnitude of the **cosine of the angle** between them, with the range 0 to 1 mapped from white to black.
- The cosine of the angle between two vectors  $a$  and  $b$  is obtained by:

$$\cos \alpha = \frac{ab}{|a||b|}$$

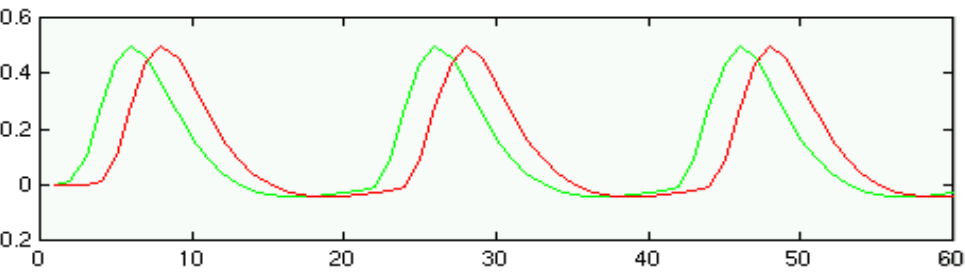
- For **zero-mean vectors**, the cosine of the angle between the vectors is the same as the **correlation** between the two variates:

$$\cos \alpha = \text{corr}_{a,b}$$

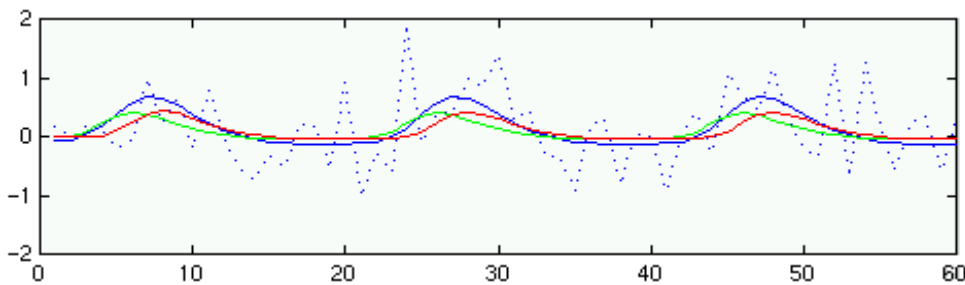
# Correlated regressors



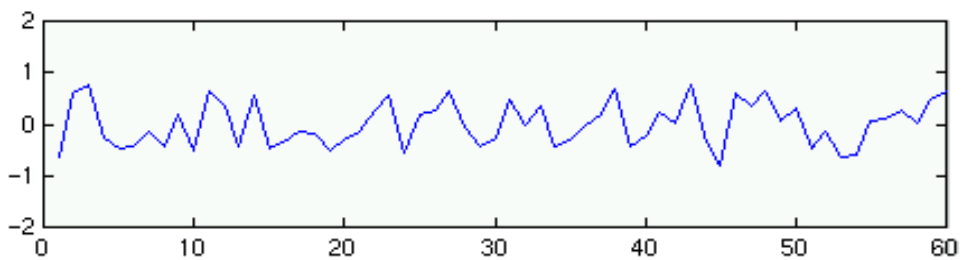
True signal



Model (green and red)

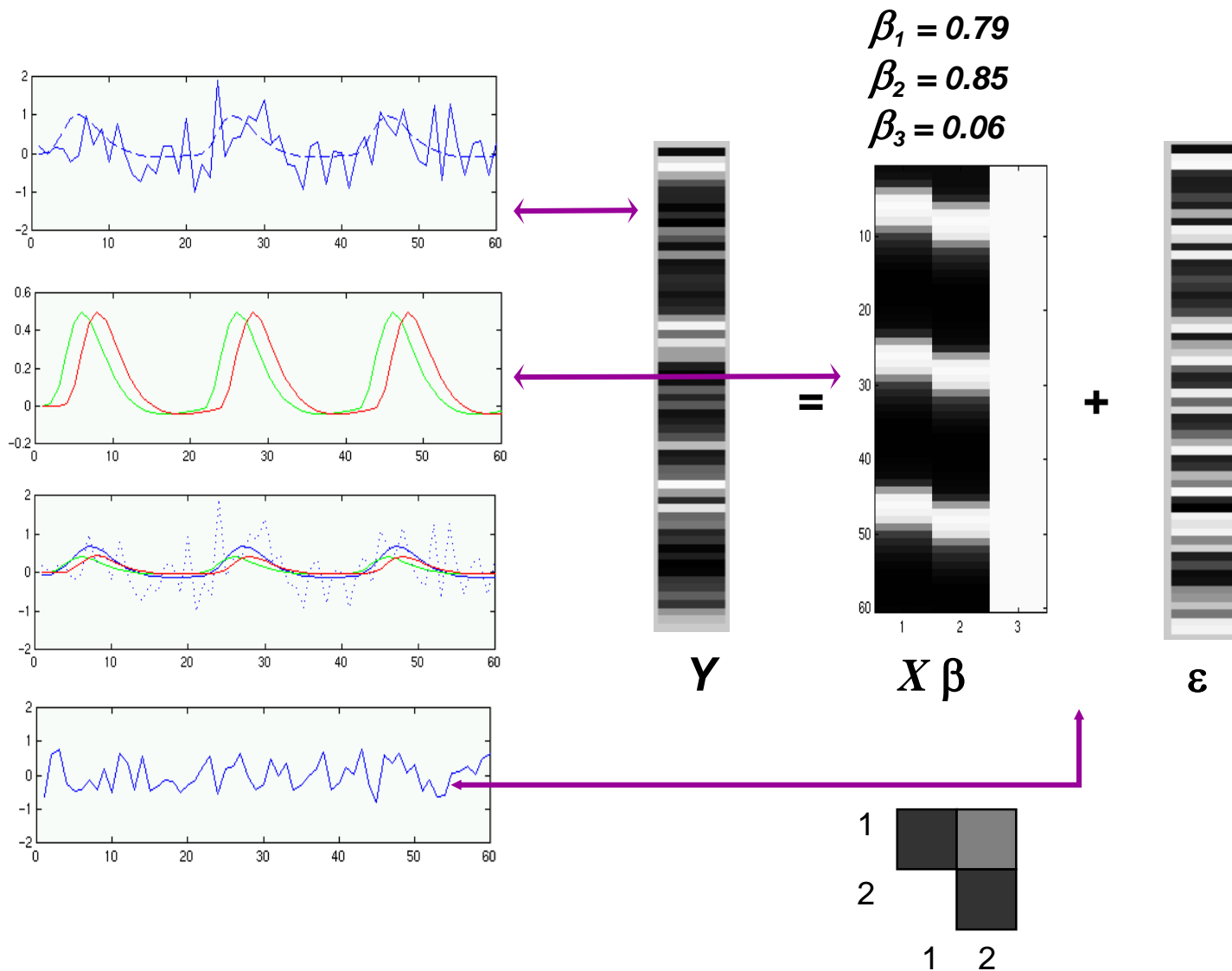


Fit (blue: total fit)



Residual

# Correlated regressors



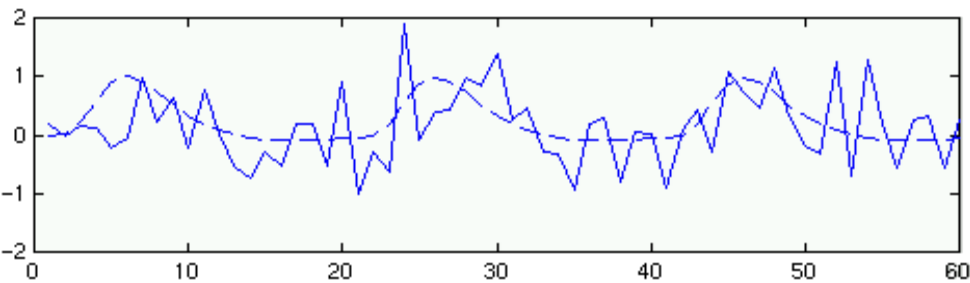
*Residual var.* = 0.3

$p(Y/\mathbf{b}_1 = 0) \Rightarrow$   
 $p\text{-value} = 0.08$   
 ( $t$ -test)

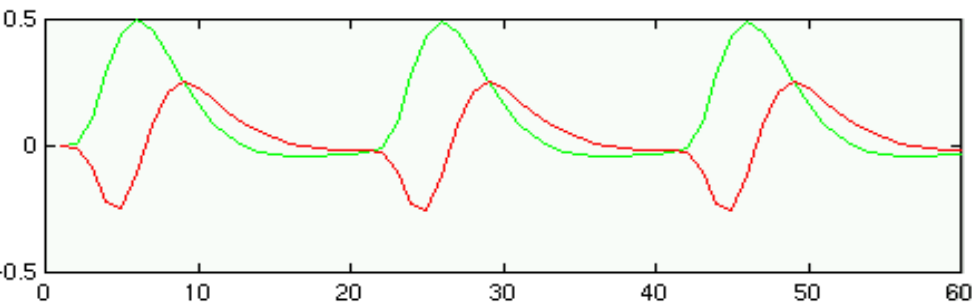
$P(Y/\mathbf{b}_2 = 0) \Rightarrow$   
 $p\text{-value} = 0.07$   
 ( $t$ -test)

$p(Y/\mathbf{b}_1 = 0, \mathbf{b}_2 = 0) \Rightarrow$   
 $p\text{-value} = 0.002$   
 ( $F$ -test)

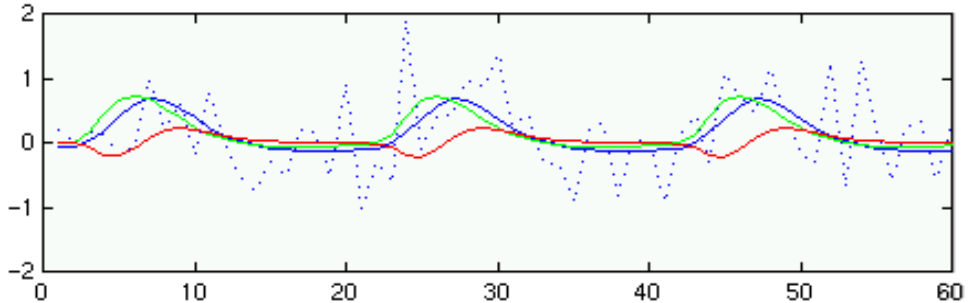
# After orthogonalisation



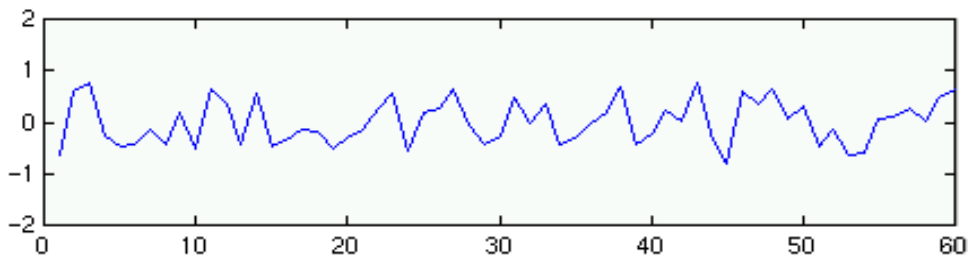
True signal



Model (green and red)  
red regressor has been  
orthogonalised with respect to the green  
one  
 $\Leftrightarrow$  remove everything that correlates with  
the green regressor

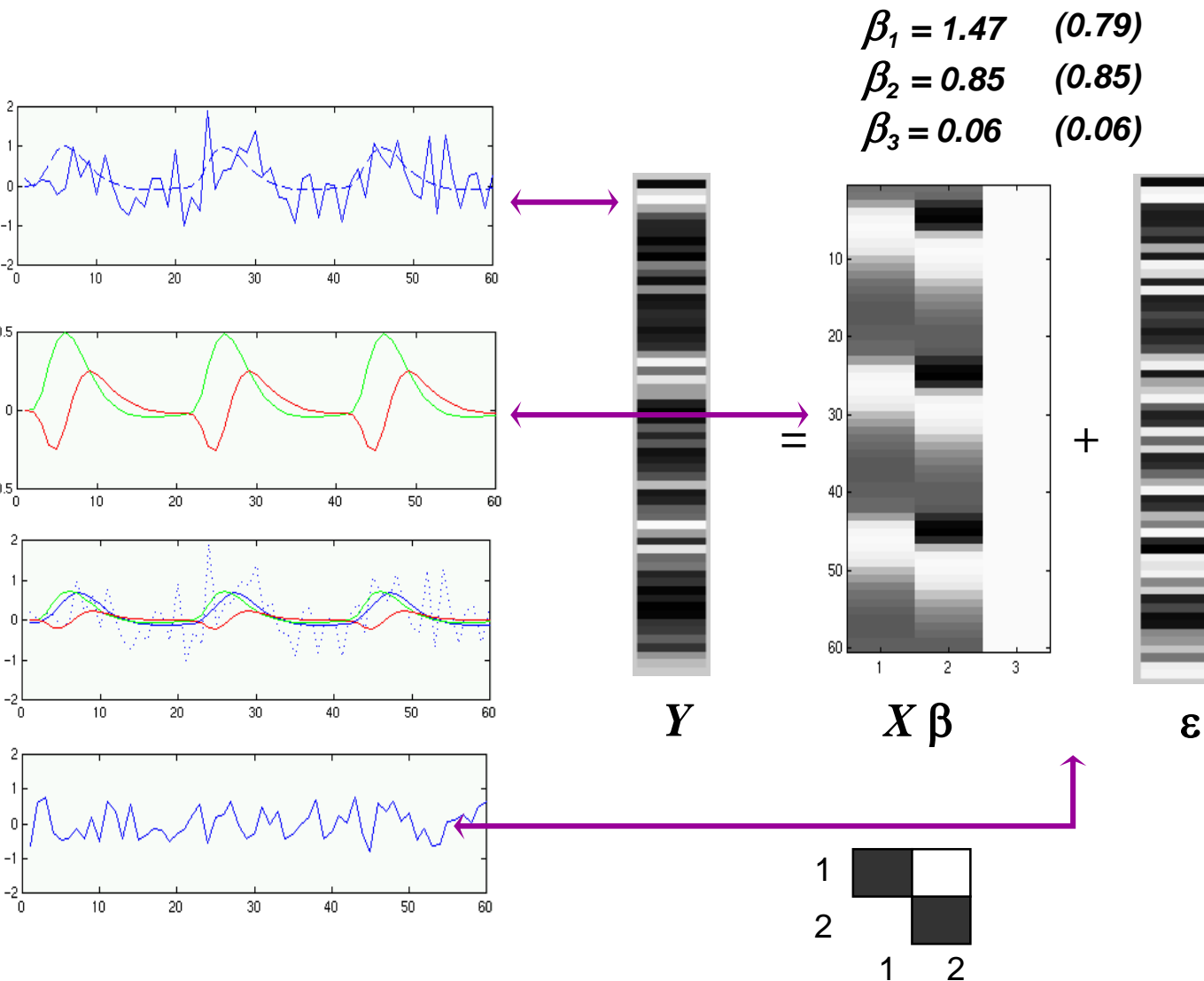


Fit (does not change)



Residuals (do not change)

# After orthogonalisation



*Residual var. = 0.3*

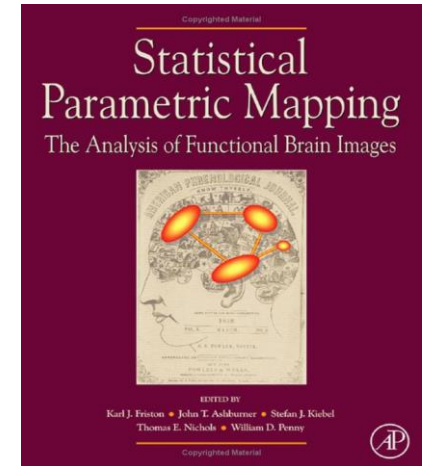
$p(Y/ \mathbf{b}_1 = 0)$   
 $p\text{-value} = 0.0003$  does change  
 ( $t$ -test)

$p(Y/ \mathbf{b}_2 = 0)$   
 $p\text{-value} = 0.07$  does not change  
 ( $t$ -test)

$p(Y/ \mathbf{b}_1 = 0, \mathbf{b}_2 = 0)$   
 $p\text{-value} = 0.002$  does not change  
 ( $F$ -test)

# Bibliography

- Friston KJ et al. (2007) *Statistical Parametric Mapping: The Analysis of Functional Brain Images*. Elsevier.



- Christensen R (1996) *Plane Answers to Complex Questions: The Theory of Linear Models*. Springer.
- Friston KJ et al. (1995) Statistical parametric maps in functional imaging: a general linear approach. *Human Brain Mapping* 2: 189-210.

**Thank you**