



Noise Models and Correction for fMRI

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- an Introduction to the PhysIO Toolbox

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The Goal of Noise Correction



Correction

The Goal of Noise Correction





Reminder: fMRI Data is noisy...









fMRI Data is noisy...



Interest in fluctuations only: Subtract the mean





Previously...



- How we ended 6 weeks ago (after preprocessing)
- After smoothing...still some fluctuation





Sources of Noise in fMRI



1	Acquisition Timing	Temporal Preproc	•	Slice-Timing
	Subject Motion	Spatial Preproc	•	Realignment
	Anatomical Identity	Spatial Preproc		Co-registration
	Inter-subject variability	Spatial Preproc	-	Segmentation
	Thermal Noise	Spatial Preproc	•	Smoothing
	Physiological Noise	Noise Modeling	•	PhysIO Toolbox

Previously....(continued)



- ResMS image (cf. GLM lecture)
- Indicates where model incomplete...
- limits sensitivity...







 $\widehat{\sigma^2} = \frac{(Y - X\beta)^2}{N - p}$

Outline – Noise Correction



- MRI Time Series Recap and Noise Sources
 - Why de-noising? Structured Noise; Noise Pathways
- Noise Correction Approaches
 - Target: Scanner Drift, Motion, Cardiac/Breathing Cycle
 - Method: Modeling VS Preprocessing
 - Input: fMRI Data VS Peripheral Measures
- Prospects for Improving Group Statistics
- Limitations
 - Degrees of Freedom; Task-related "noise"; Interoception

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fMRI = Acquiring Movies



- The Localized Time-series is the Fundamental Information Unit of fMRI
- Signal: Fluctuation through Blood oxygen level dependent (BOLD) contrast

Noise: All other fluctuations

Run/Session: Time Series of Images



scan 1

time

••



Noise Categories & Reduction

- Thermal Noise
 - temporally uncorrelated
 - reduced SNR → risk of false negatives
 - Remedy: Spatial Smoothing
- Noise: All other fluctuations
- "Structured" Noise
 - temporally correlated
 - reduced SNR \rightarrow risk of false negatives
 - correlated with task \rightarrow risk of false positives
 - Remedy: Noise modeling (e.g. GLM)



Inference = Signal-To-Noise

$$t = \frac{\beta}{\sqrt{\sigma_{\varepsilon}^2 (X^T X)^{-1}}} = \frac{\beta \| \boldsymbol{x} \|}{\sigma_{\varepsilon}}$$

$$F = \frac{N - M}{M_1} \cdot \frac{(\sigma_s^2 + \sigma_N^2) - \sigma_N^2}{\sigma_N^2}$$

Recap: MR Image Encoding





Image Reconstruction & Noise





- Image reconstruction is also a huge GLM, ~10⁵-10⁶ rows
 - 3 mm slice, 8 chan: 64²*8 = 512k
 - 1 mm slice, 32 ch: $256^{2*}32 = 2M$
- Any change between volumes in encoding matrix (field), object magnetization and thermally induces image noise

$$\widehat{m} = \left(E^H E\right)^{-1} E^H s$$



What fluctuates?





Structured Noise in MRI





The Problem: Physiological Noise 57



The Problem: Physiological Noise **T**

Cardiac effects

- Systole:
 - Blood pumped into brain, vessel
 volume increases: pulsatile vessels
 - CSF pushed down: pulsatile CSF
- Diastole:
 - Vessel volume decreases
 - CSF flows back into "void" brain volume

A Cardiac Cycle in the Brain



The Problem: Physiological Noise 57



The Problem: Physiological Noise 57

Cardiac effects











Vessel Anatomy



Locations of Fluctuations

The Problem: Physiological Noise **T**





- Respiratory effects
 - Chest (&head) moves with respiratory cycle
 - Changes in lung volume change encoding magnetic field for MR
 - Geometric distortion/scaling
 - Respiratory-sinus arrythmia
 - Heart beats faster during inhalation

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Noise Correction Targets





Drifts: High-Pass Filtering

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- Discrete Cosine Model (last lecture) of slow oscillations (cycle ≥ 128 s)
- Was: Extra, non-task related columns in design matrix: nuisance regressors
- Now: Part of "hidden" preprocessing
 - Residual forming Matrix

$$K = 1 - X_0 (X_0^T X_0)^{-1} X_0^T$$

- With X_0 being the design matrix modeling the confounds
- In fact, GLM in SPM estimates $K \cdot \mathbf{y} = K \cdot X \cdot \mathbf{\beta} + K \cdot \varepsilon$

Modeling VS Preprocessing



- Modeling:
 - Filters, projections (e.g. to independent components) etc. are all linear operations
 - Combination in one design matrix, together with task
 - Simple test of correction efficacy: F-test on nuisance regressors
- Preprocessing:
 - The data y entering the GLM is altered $\Rightarrow y' = X\beta + \varepsilon$
 - For non-linear changes of y or inter-voxel dependencies, alteration outside GLM necessary

The Problem with Preprocessing 50

- Problem: No inherent measure of efficacy (F-test in GLM), correlation with task regressors undetected
- "Advantage": No loss of degrees of freedom (sensitivity of F-test)
 - But it it only a hidden loss, statistics for inference is biased, if performed modeling is not incorporated
- Modeling via GLM recommended, if possible
 - Drifts, Motion Regressors
 - RETROICOR, HRV, RVT
 - aCompCor, (ICA)

Motion: Preprocess & Modeling

- Correction for motion artifacts is actually a combination of Preprocessing and modeling
- Preprocessing cannot correct spin-history effects, intravolume movements (non-rigid!), small partial volume effects
- Preprocessing:
 - Realignment
 - Motion "Scrubbing"
- Modeling (from estimated realignment parameters)
 - Retrospective Modeling: Motion Regressors
 - Motion Censoring

Retrospective Motion Correction

- Best: Avoid subject motion in the first place
- Better: Use Prospective Motion Correction
- Standard: Perform rigid-body realignment, use parameters as nuisance regressors
 - 6 parameters: translation+rotation
 - 12 parameters: include derivatives (for temporal shifts)
 - 24 parameters: include squared regressors
- 24-parameter model known as Volterra expansion

Friston, MRM, 1996

Motion Censoring = "Scrubbing"

- Detect outlier volumes (strong movement, but also spikes, RF flip angle fluctuations)
- Inform the GLM of these bad volumes via stick regressors (zero everywhere else, 1 at volume)
 - Will absorb all variance of that volume
- Problem: Temporal filtering before GLM might create
 Gibbs ringing of outliers into neighbors
- Alternative: censoring during preprocessing
 - interpolate faulty volume by neighbors

Noise Correction Targets





Image-based Noise Correction



Model-based Phys Noise Correction



Noise Modeling



RETROspective
Image CORrectionCardiac Response
FunctionRespiratory
Response Function• Cardiac/respiratory
phase• Heart Rate
 φ_c • Resp. Volume
per Time

Fourier expansionconvolved withconvolved with(cosine/sine)CRFRRF

evaluated at 1 time point (slice) per volume =

regressor

Noise Modeling





Model: Fourier Phase Expansion

- Cosine and sine to allow for constant phase shifts per voxel
- Higher model orders to account for under-sampling of physiological frequencies with typical TR in fMRI



Aliasing of Physiology





Courtesy: R. Birn, HBM 2015

Noise Modeling





Noise Modeling





Exploratory Phys Noise Correction



Noise Component Modeling



- Use priors about physiological noise to identify noise components (time series)
 - Spatial Priors: Mechanisms of physiological noise implicate physiological noise in CSF, blood vessels
 - Temporal Priors: Knowledge about typical physiological frequency contents (heart ~ 1Hz, breathing 0.2-0.4 Hz)
 - Note that simple filtering is impossible (cf. aliasing)
 - Population Priors: Use dictionary learning from manually labelled training set of subjects (FIX)

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Spatial ICA	FIX	CORSICA	aCompCor		
(Thomas et al.,	(Salimi-Khorshidi	(Perlbarg et	(Behzadi et al.,		
2002)	et al., 2014)	al., 2007)	2007)		
Breathing &	Multi-subject	CSF Pools (Flow)			
Cardiac Frequency	dictionary	Vessels (Pulsation)			
(~0.25 Hz, ~1 Hz)	(hierarchical	White Matter (non-BOLD)			
	classifier)				
	J = /				

PCA VS ICA



- Methods to extract components (i.e. summarize ROIs/spectra) differ:
 - Maximum variance time series: Principal Component Analysis (PCA) from region of interest (aCompCor, Behzadi 2007)
 - Maximally independent time courses/sites: spatial/temporal ICA, FSL MELODIC, FIX
- aCompCor is basically identical to a seed-based correlation analysis in resting-state fMRI
 - Here: seed is in region-of-no-interest and correlated time series regressed out
 - See previous talk (resting state analysis) for more details

Preprocessing Techniques







Other Physiological Corrections

- Non-linear models
 - DRIFTER: Kalman Filter, Bayesian, *Joint* Stochastic State-space model of peripheral physiology and BOLD
- Identify noise via task test-retest reproducibility
 - PHYCAA: e.g. via high-freq. autocorrelation, anatomy
 - GLMDenoise: PCA of noise regressors
- MEICA: Multi-Echo ICA
 - Use diff. TE-images to decompose proton density from T2* changes

Särkkä, Neurolmage, 2012 Churchill, Neurolmage, 2012/13 Kay, Front. Neurosc., 2013 Olafsson, Neurolmage, 2015

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When? – Literature Evidence



Resting-state:

- Birn, R. M. "The Role of Physiological Noise in Resting-state Functional Connectivity." *NeuroImage 62*, 2012
- Birn, R. M., et al. "Separating Respiratory-variation-related
 Fluctuations from Neuronal-activityrelated Fluctuations in fMRI." *NeuroImage 31*, 2006

C Resting-state correlation



D Rest-state corr – after RVTcor



Task-based:

Hutton, C., et al. "The Impact of Physiological Noise Correction on fMRI at 7 T." *NeuroImage 57*, 2011:



All these methods, but...



 Physiological noise correction not a default preprocessing step in task-based fMRI

Reasons

Impact on group level fMRI

no reports for non-trivial paradigms

- Existing Toolboxes lack...
 - robust, automatic implementation
 - dealing with variable peripheral data quality

Paradigm: Learning from Advice

- Hierarchical learning of trustworthyness of advisor over time
- Contrasts: Prediction and Prediction Error about advice



recommendations of adviser were **veridical** (pre-recorded videos from behavioural study)

volatility of advice (changing intentions of adviser through incentive structure)

interactive, gender-matched (**40** male subjects)

fMRI design: Philips Achieva 3T TR/TE 2500/36ms, 2 x 2 x 3 mm³

Diaconescu et al, 2014, PLoS Comp. Biol.

Group Level Impact PhysIO



- Andreea Diaconescu (TNU): Social Learning Experiment 2012-2014, (N=35)
- F-contrast: Where does physiological noise model explain significant variance?



Relevance for Neuromodulation

cardiac (red), respiratory (blue), cardXresp (green)



Relevance for Neuromodulation

VTA (DA)

Raphe Nuclei (5-HT)

J

Locus coeruleus (NA)

Effects on Group Contrasts

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Limitations of Noise Modeling

- Degrees of freedom, sensitivity reduced by too many ineffective regressors
 - F-test informative
- Intrinsic correlations of functional areas of interoception and peripheral physiology
 - E.g. Amygdala, Insula, ACC
 - Controversial reading:
 <u>fMRI of the Amygdala: All In Vein? Neuroskeptic</u>
 - Alternative: Masking, Pure anatomical priors removing CSF, angiography (vessels)

Conclusion



- MRI Time Series and Physiological Noise
- Image-Based Correction in the GLM
- Noise Modeling Prospects: Group FX

The PhysIO Toolbox

- Structured noise through cardiac/resp cycle (70%)
- Nuisance regressors from
 Fourier expansion, response functions
- Increase group sensitivity (low inter-subject variability), fewer false positives
- Correction in SPM/Matlab in practice => NOW!



- Demo: The PhysIO Toolbox for Physiological Noise
 Correction in fMRI
 - Features and Workflow
 - Image-based physiological noise correction in the GLM
 - RETROICOR, HRV, RVT
 - Noise-ROIs
 - Practical Demo (SPM Batch)
 - Estimating different Models
 - Understanding the Preprocessing Plots
 - Automatic Model Assessment, Diagnostics on Contrast

Image-based Noise Correction



The PhysIO Toolbox

- Developed at the Translational Neuromodeling Unit (TNU) since 2008
 - Lead programmer: Lars Kasper (TNU)
 - Contributors: Jakob Heinzle (TNU), Steffen Bollmann (KiSpi Zurich)
- Part of the TNU «TAPAS» software suite
- Used at the TNU, in Zurich and beyond by ~50 researchers
 - Iglesias 2013, Neuron; Kasper 2014, NeuroImage; Bollmann 2014, PhDThesis; Sulzer 2013, NeuroImage; Hauser 2014, NeuroImage; Grueschow 2015, Neuron
- Download & Example Data:
 - <u>https://www.tnu.ethz.ch/en/software/tapas.html</u>
 - https://www.tnu.ethz.ch/en/software/tapas/data.html



Workflow of the PhysIO Toolbox **T**



Flowchart of Noise Correction





Scan Sync with Philips Gradients



Data Preprocessing Overview





Preprocessing: Peak Detection



Peak Detection: Robustness





Noise Modeling





Diagnostics: Model Assessment





Model Check: SPM F-contrasts





Finally: No

Check Influence of Physiological Noise (Correction) on Data

- SPM
- F-contrast on 1st and second level

Flexibility: Scanner vendors





References



Birn, Rasmus M., Jason B. Diamond, Monica A. Smith, and Peter A. Bandettini. 2006. "Separating Respiratory-variation-related Fluctuations from Neuronal-activity-related Fluctuations in fMRI." NeuroImage 31 (4) (July 15): 1536–1548. doi:10.1016/j.neuroimage.2006.02.048.

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Harvey, Ann K., Kyle T.S. Pattinson, Jonathan C.W. Brooks, Stephen D. Mayhew, Mark Jenkinson, and Richard G. Wise. 2008. "Brainstem Functional Magnetic Resonance Imaging: Disentangling Signal from Physiological Noise." Journal of Magnetic Resonance Imaging 28 (6): 1337–1344. doi:10.1002/jmri.21623.

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fMRI = Acquiring Movies



